

# Nanomedicine: from high tech to global health

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***Robert K. Prud'homme,***

***Brian Johnson, Walid Saad, Ying Liu, Marian Gindy, Stephanie Budijono,  
Margarita Herrera-Alonso, Varun Kumar, Suzanne D'Addio, Robby Pagels, Chet  
Markwalter, Brian Wilson, Kurt Ristroph***

***Dept. Chemical Engineering  
Princeton University***

***Support: NSF, NIH, Gates Foundation, BASF, Evonik, Merck, J&J, GSK,  
Celator, Optimeos; SEAS Helen Hunt, Innovation Forum, Nanomedicine  
for BBB-crossing in CNS oncologic pathologies MAECI PROJECT  
2019-2021***

# Enhanced Bioavailability Using Scalable Flash NanoPrecipitation

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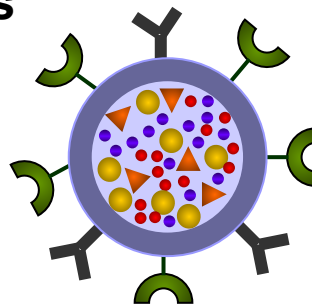
# Outline

1. ***Nanoparticles by turbulent micromixing in confined impinging jet mixers (CIJ): FNP, MIVM***
  1. *Development of an idea: Flash NanoPrecipitation (FNP)*
2. ***Nanoparticle drug delivery***
  1. ***Oral: increased bioavailability (Gates funding)***
  2. ***Parenteral: Controlled release with conjugation***
  3. ***Parenteral: Ion pairing for hydrophilic drugs (LNPs RNA, peptides, proteins)***
3. ***mRNA and DNA Lipid Nanoparticles: Targeting***

# Next Generation Nanoparticles (NPs)

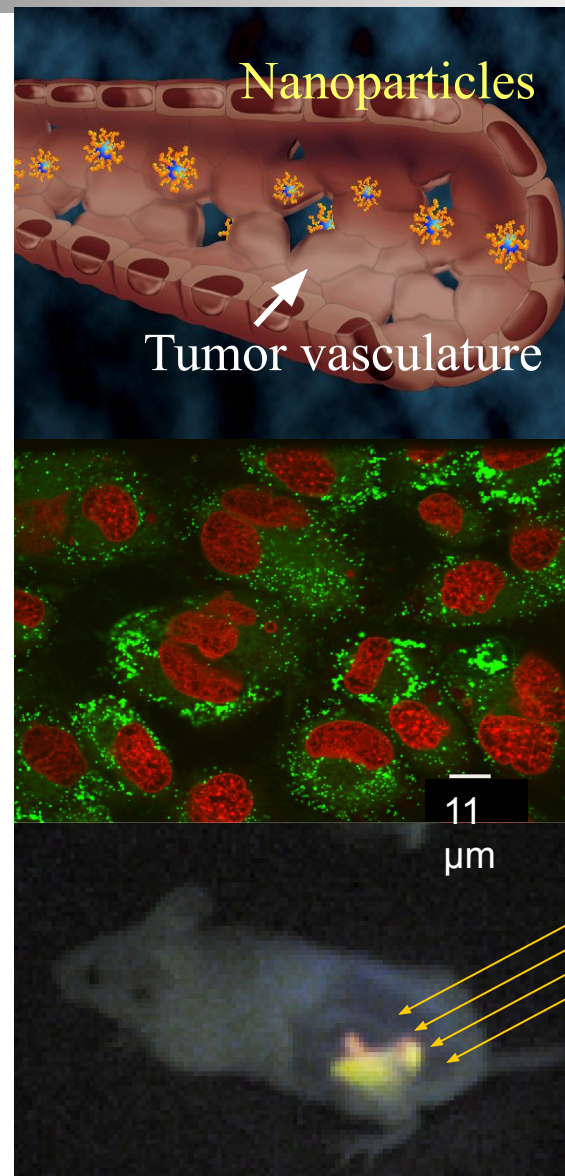
## Motivation

- Bioavailability: 40% of new drug compounds are hydrophobic
- EPR targeting of solid tumors
- Targeting toxic API
- Multiple drugs cocktails
- Imaging where toxic APIs go
- siRNA, mRNA, proteins and peptide delivery



## More than just small

- Size
- Surface functionality
- Stoichiometric encapsulation of multiple species: cocktails
  - Imaging plus delivery
  - Targeting plus delivery
- Scalable and manufacturable



# Next Generation Nanoparticles (NPs)

## Motivation

*"...over the next few years some of the complex theranostic strategies published rampantly in chemistry journals will fall out of contention...For me, something that's too difficult to make or too complex to sustain in large-scale production is not what we are interested in."*

*J.Janijic C&EN Sept 26,2011.*



**Scott McNeil**, the head of the National Cancer Institute's Nanotechnology Laboratory

*"Another big hurdle in developing nanomedicines is **scaling up** the synthesis of the particles ....**developing a synthesis that yields particles ... on a consistent basis. That is still a difficult process.**" (C&ENews. ACS.org, June 20, 2016, p. 19)*

# Next Generation Nanoparticles (NPs)

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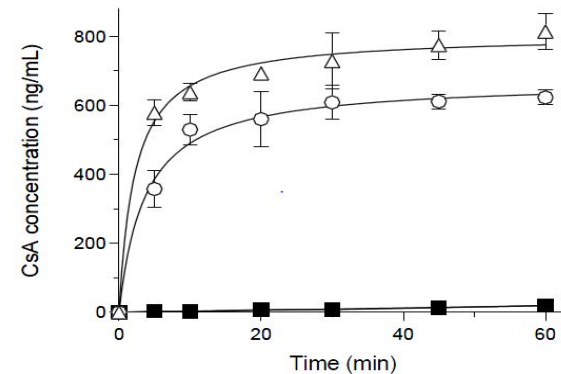
# Conflicting Goals: Oral vs Parenteral Delivery

## Schizophrenic communities

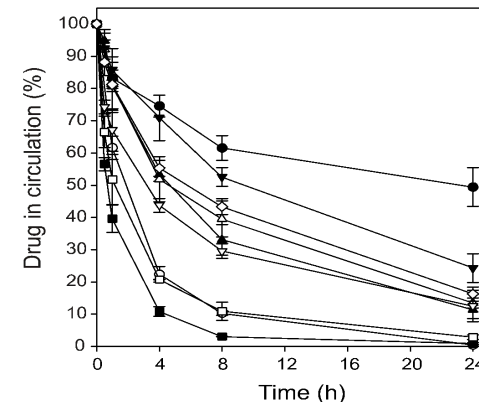
### 1. Increased bioavailability

1. **Oral: Gates global health drugs**
2. Milling and Solid Spray Dried Dispersions (Bend Res.): make things smaller, amorphous
3. Make things dissolve more rapidly

- Cyclosporine A
- NPs ~200-300 nm
- Ppt with lecithin + mannitol and spray dried
- Supersaturations of 100  
(Sato, Prud'homme *Intl.J.Pharm* (2017))

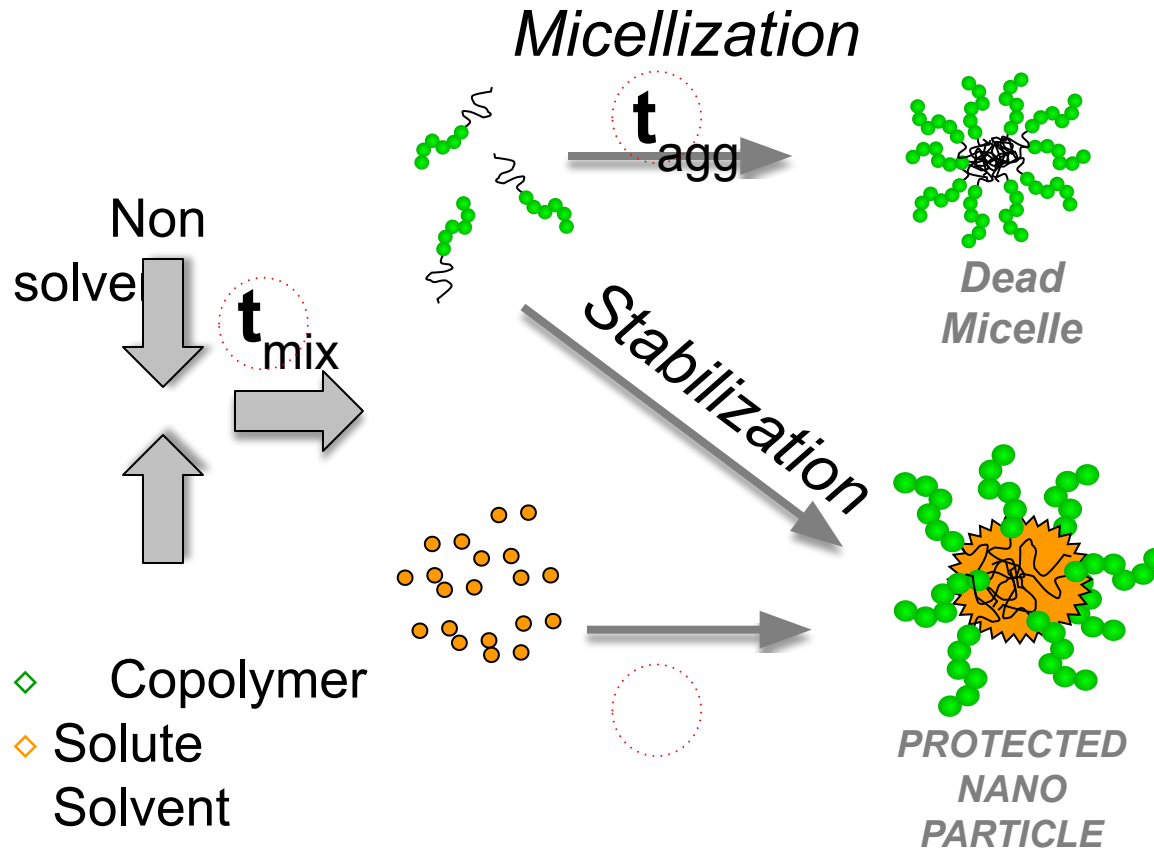


- Paclitaxel conjugate
- NPs 60 nm
- (Ansel, Prud'homme *Mol Pharm* (2102))



# Nanoparticle formation by Flash NanoPrecipitation

## *Block copolymer directed rapid precipitation*



Johnson, Prud'homme AICHE J (2003), Liu, Prud'homme, Fox, Chem Engr. Sci. (2003)

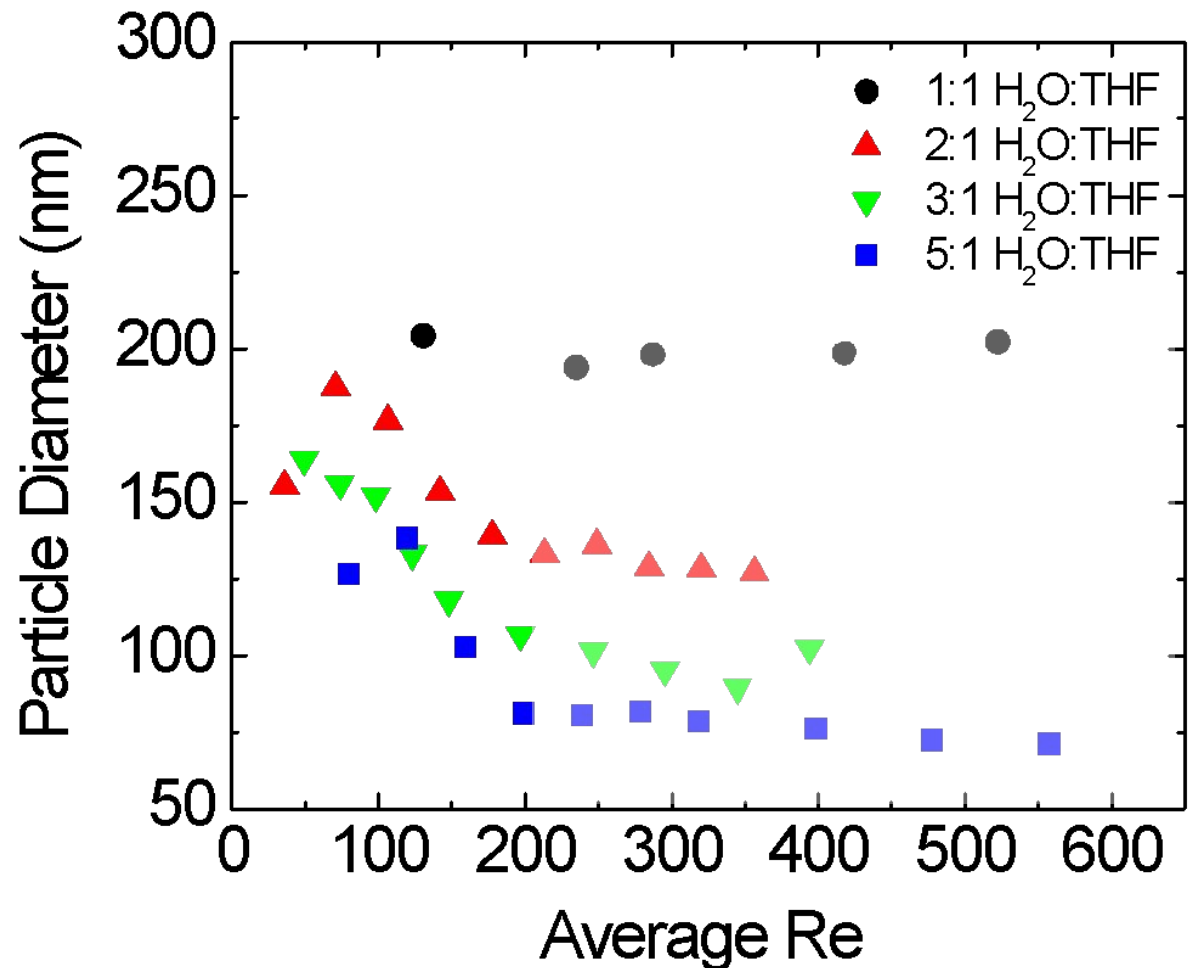


# Control of particle size

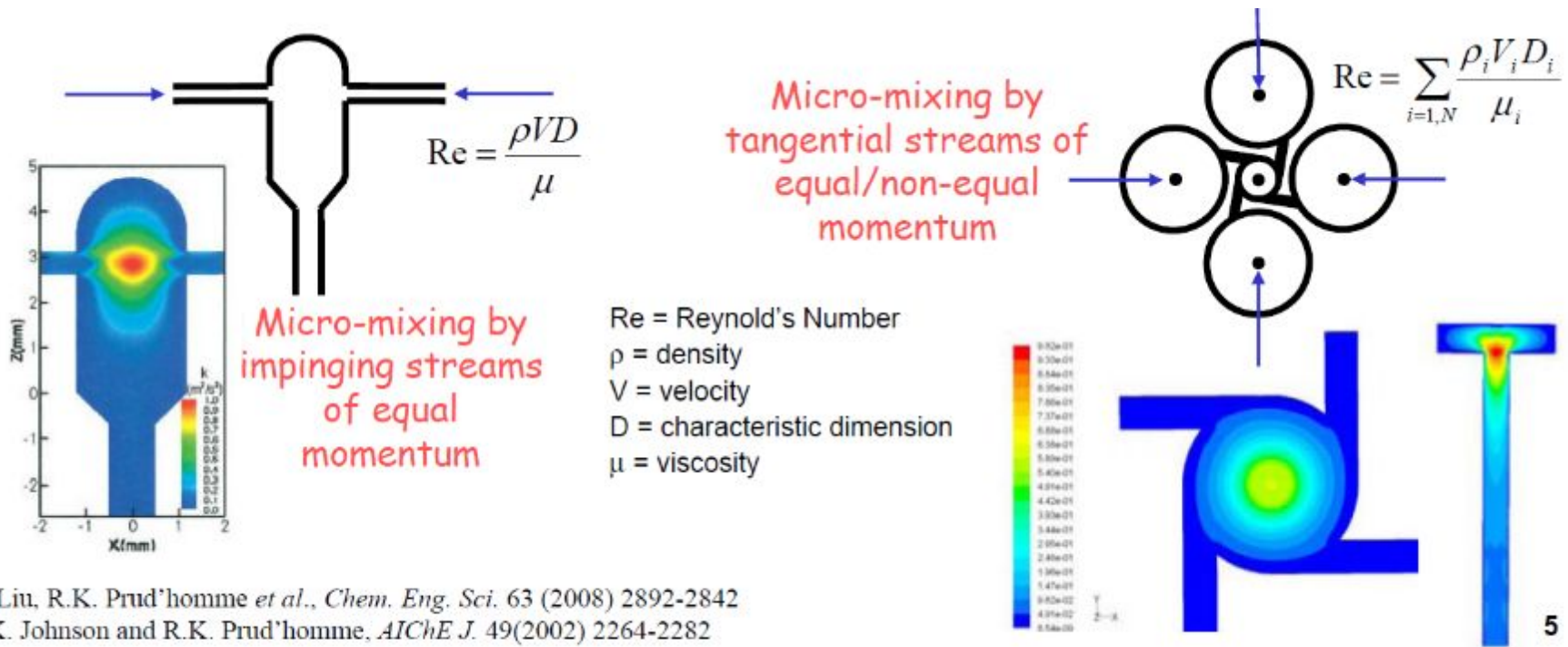
## 1. *Mixing intensity*

## 2. *Super-saturation*

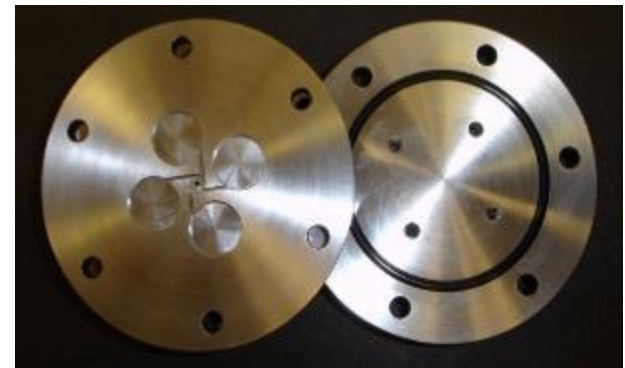
- *Control super-saturation by changing solvent quality or solute concentration.*
- *Higher super saturation leads to smaller particles*



# Confined impinging jet micro-reactors



Y. Liu, R.K. Prud'homme *et al.*, *Chem. Eng. Sci.* 63 (2008) 2892-2842  
 B.K. Johnson and R.K. Prud'homme, *AIChE J.* 49(2002) 2264-2282



# Princeton CIJ mixers and COVID vaccines

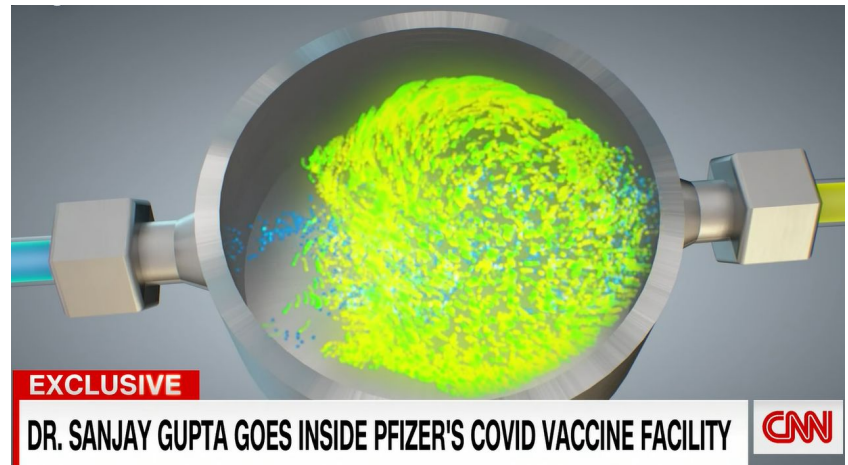
Pfizer BioNTech COVID vaccine have produced 3 billion doses

Mike McDermott, the President of Pfizer Global Supply, in the CNN interview where they took the press through the Pfizer production process: **“the impingement jet mixer makes it possible.”**

CNN. *Manufacturing moonshot: How Pfizer makes its millions of Covid-19 vaccine doses*  
<https://www.cnn.com/2021/03/31/health/pfizer-vaccine-manufacturing/index.html>.

Johnson, Brian K., and Robert K. Prud'homme. "Chemical processing and micromixing in confined impinging jets." *AIChE Journal* 49.9 (2003): 2264-2282.

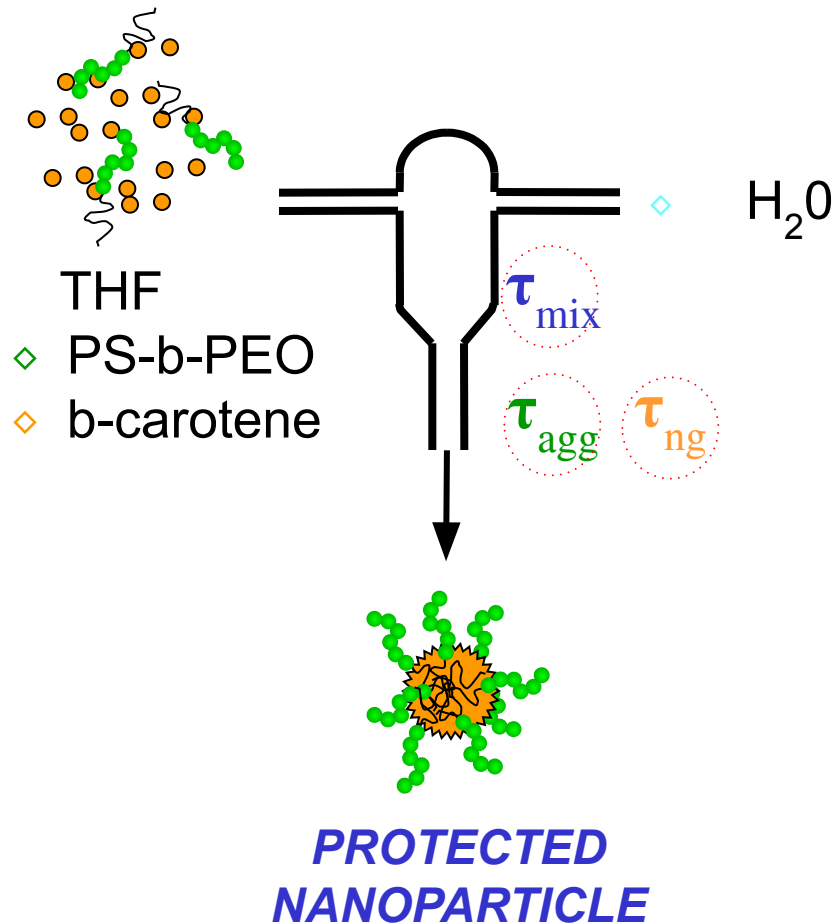
Johnson, Brian K., and Robert K. Prud'homme. "Flash nanoprecipitation of organic actives and block copolymers using a confined impinging-jets mixer." *Australian Journal of Chemistry* 56.10 (2003): 1021-1024.



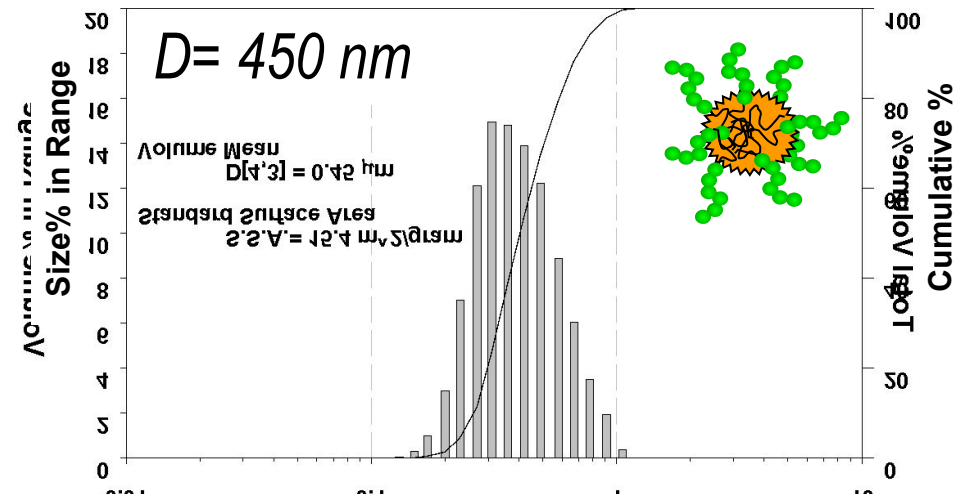
<https://fb.watch/5q7eNA3wnx>

# “FLASH” Nanoparticles Precipitation Size Control

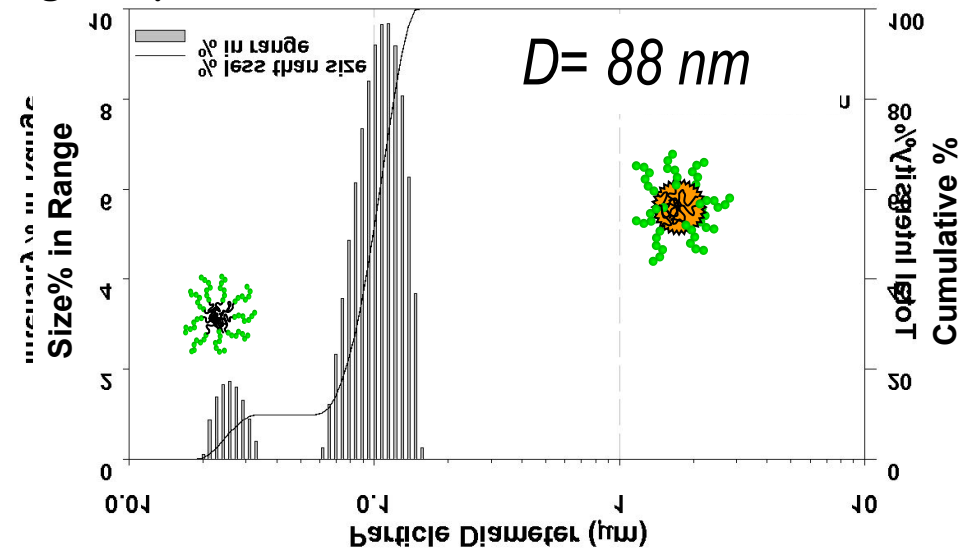
- High throughput, > 2 wt% active
- High NP loading



2.8 m/s, (2.6 wt% drug, 0.4 wt% Copolymer)

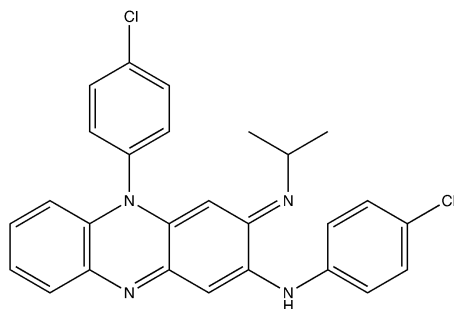


Change Inputs to Process



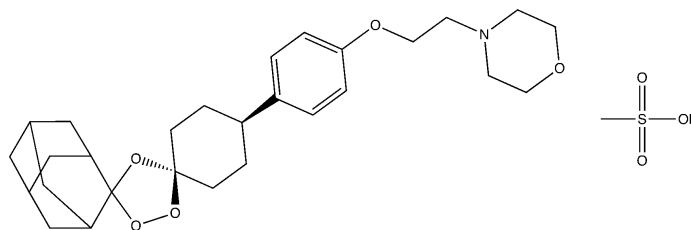
# Drugs Considered

Clofazimine



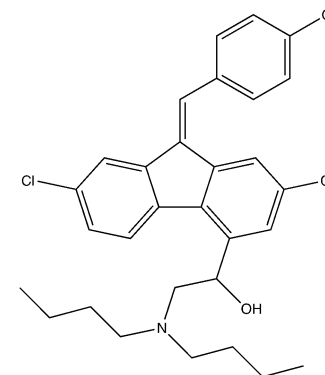
Ref: Design and Solidification of Fast-Releasing Clofazimine Nanoparticles for Treatment of Cryptosporidiosis". *Molecular Pharmaceutics*. **14**(10) 3480-3488 (2017); "Rapid Recovery of Clofazimine-loaded Nanoparticles with Long-term Storage Stability as Anti-Cryptosporidium Therapy". *ACS Applied Nano Materials*. **1**(5) 2184-2194 (2018)

OZ439



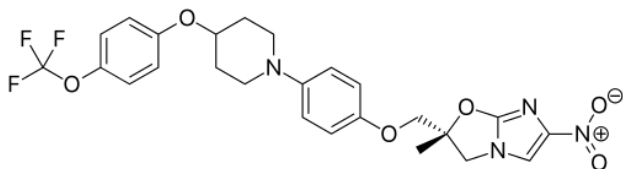
Ref: "Encapsulation of OZ439 into Nanoparticles for Supersaturated Drug Release in Oral Malaria Therapy". *ACS infectious diseases*. **4**(6) 970-979 (2018); "Spray drying OZ439 nanoparticles to form stable, water-dispersible powders for oral malaria therapy". *Journal of Translational Medicine* (2019), just accepted

Lumefantrine



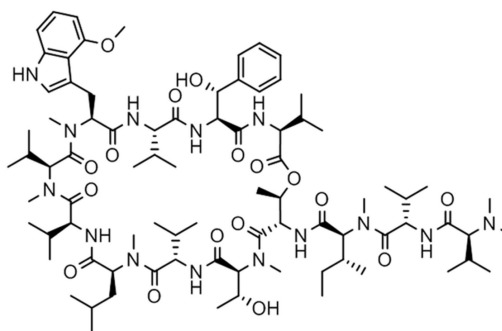
Ref: "Amorphous Nanoparticles by Self-assembly: Processing for Controlled Release of Hydrophobic Molecules". *Soft Matter*. **15** 2400-2410 (2019)

Delamanid



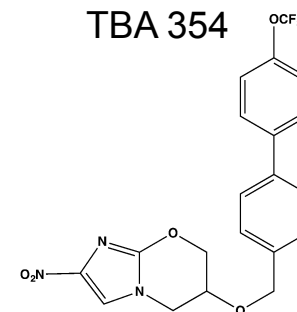
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Ecumicin



Ref:  
<https://app.box.com/s/5lggnm4tv84kcb0cry0tsch y9oszzqzi>

TBA 354



Ref:  
<https://app.box.com/s/57cromgxhg8uyqiz4zegtaf wqbclg3nk>

# Malaria is a global health pandemic

**210 Million**

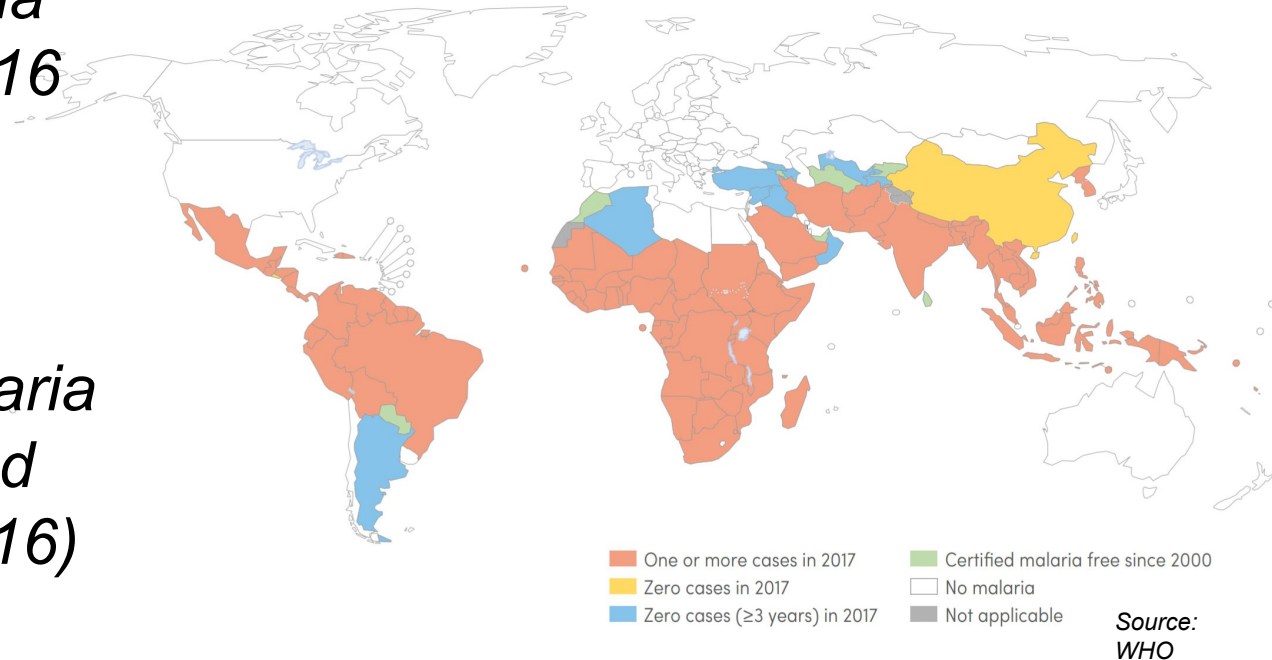
*Cases of malaria  
worldwide in 2016  
alone*

**429,000**

*Deaths due to malaria  
or malaria-related  
complications (2016)*

**>70%**

*Of deaths were in  
children under 5 years  
of age*

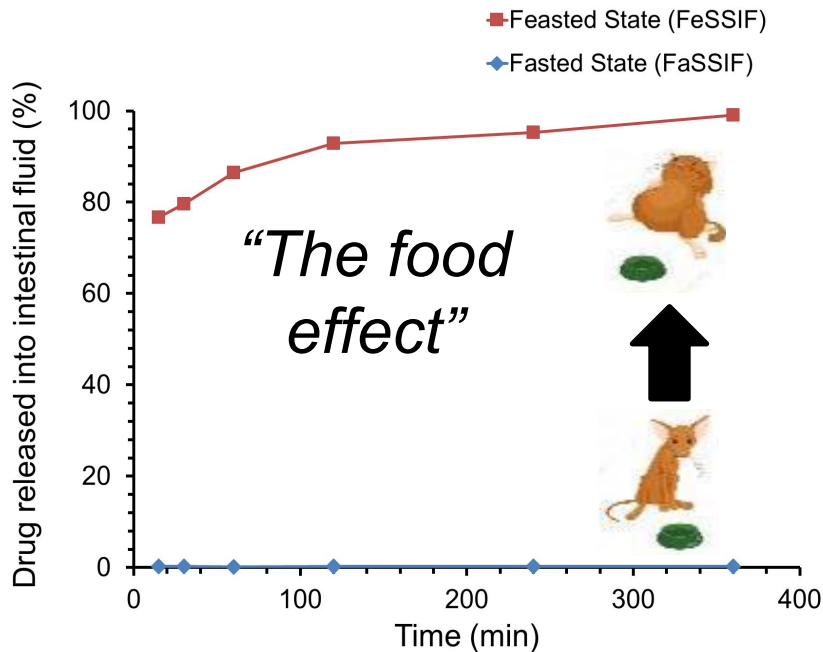




# Lumefantrine: Two pharmaceutical challenges

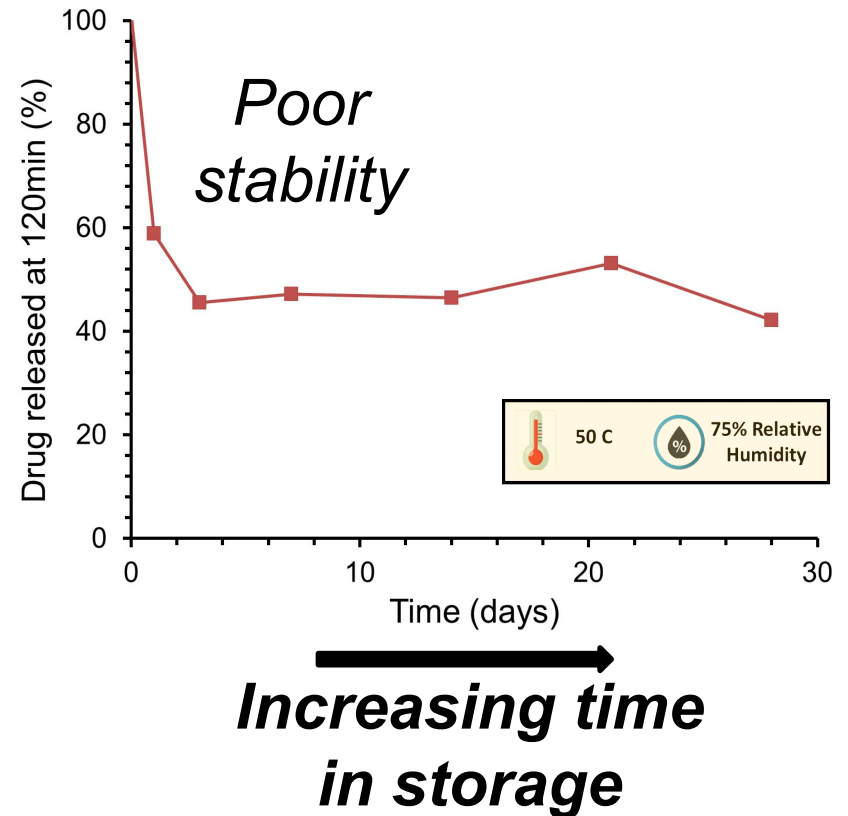
## Solid Spray Dried Dispersion

### 1 Bioavailability is dependent on food intake



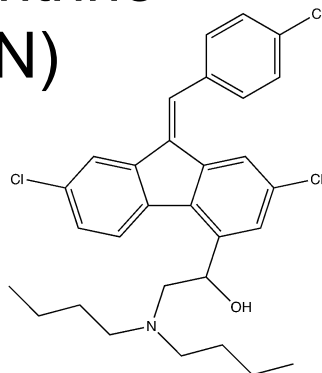
Feng et al. J Transl Med (2019), Feng et al. Soft Matter (2019)

### 2 Crystallization over time reduces shelf-life



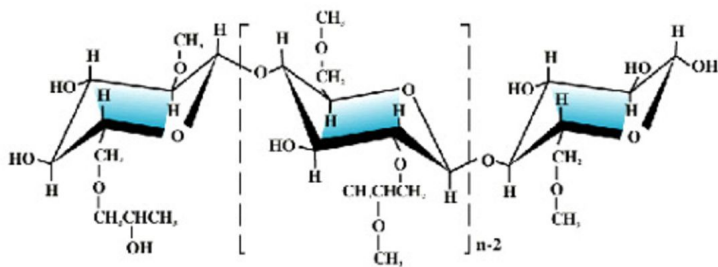
# Lumefantrine Stabilizers

## Lumefantrine (LMN)



### • HPMCAS:

- NP size: ~ 100 nm
- HPMCAS126, 716, 912 all form NPs, but 126 most stable
- 90% drug loading (60% in previous work)

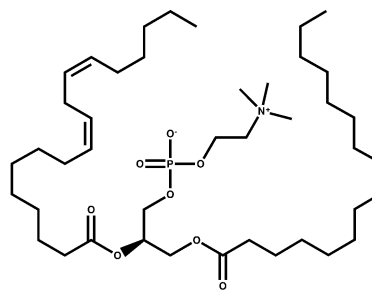


### • Lecithin:

- NP size: ~ 400 nm
- 67% drug loading
- In 10% organics (THF), stable for ~ 4-6 h

### • Zein/Casein

- NP size: ~ 200 nm
- 40% drug loading
- In 10% organics (EtOH& acetone), stable for ~ 6h



*Lecithin*

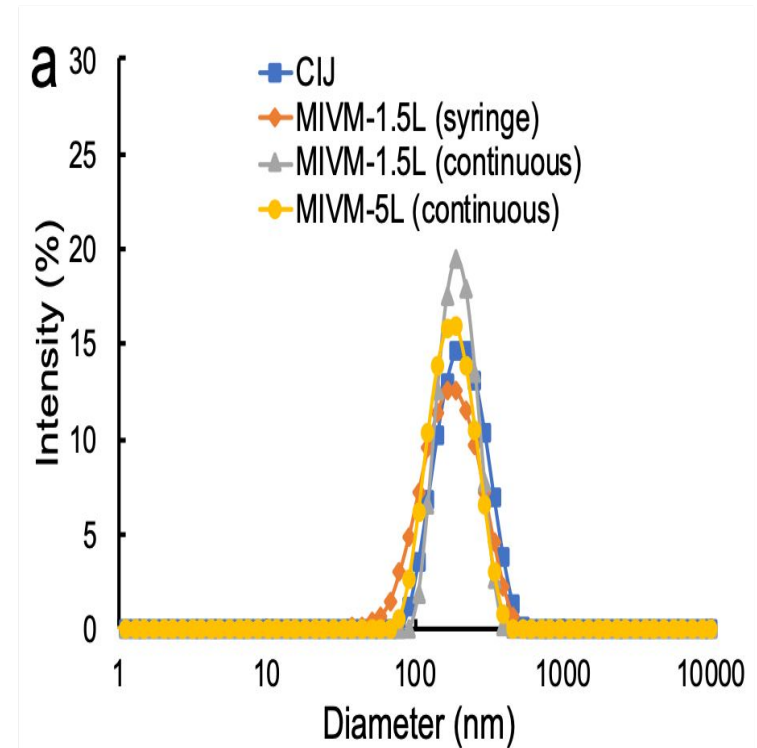
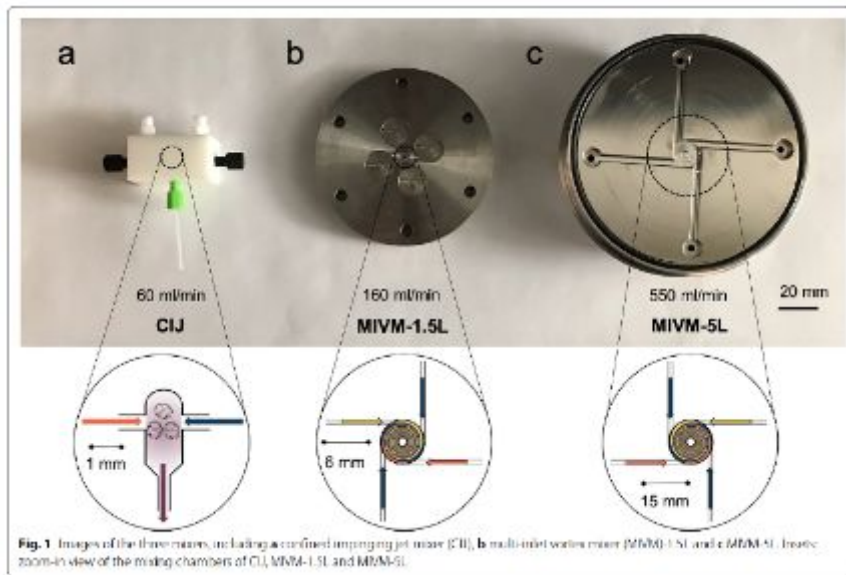


*Zein*



# SCALEUP: Equivalent NPs from 1 ml to 5 L/min)

- *Identical NPs produced at sub-mg scale to 3000 L samples*
- *Funded by the Gates Foundation*
- *GMP line developed at WuXi Aptec for global health drugs*

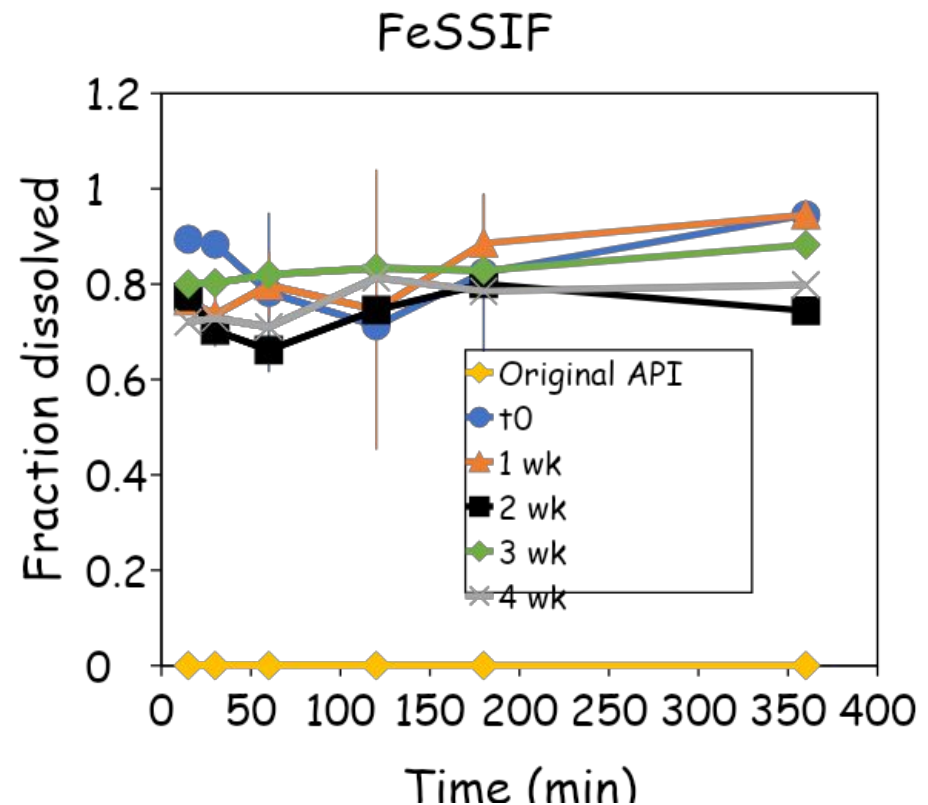
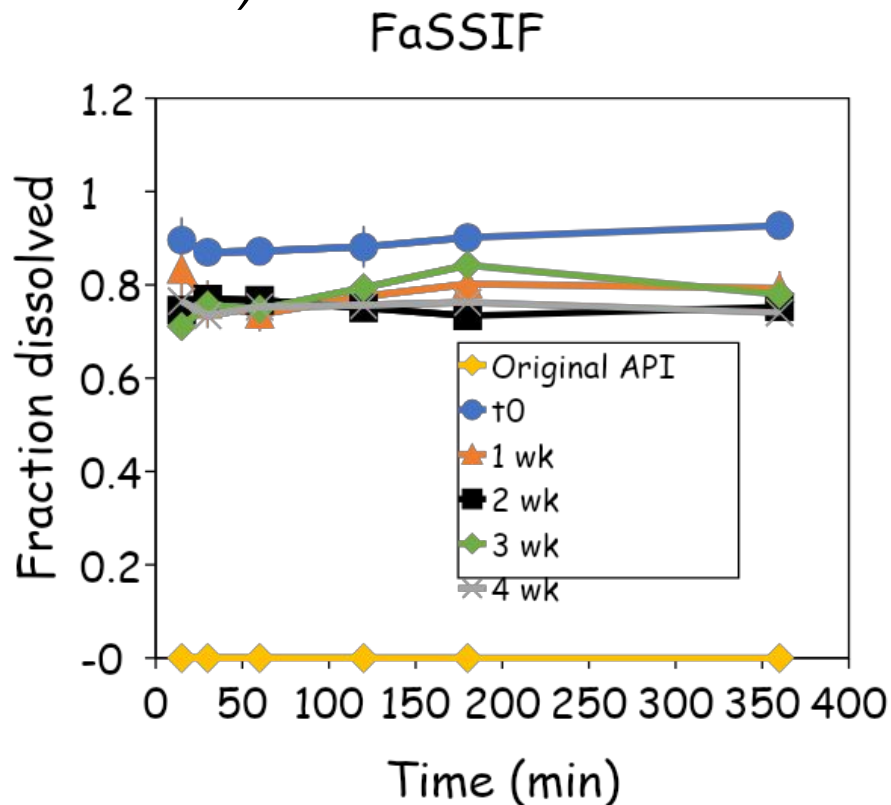


**90% DRUG LOADING IN NP**

*Armstrong J. Pharm Sci (2023)*

# Dissolution kinetics: fed/fasted state & stability

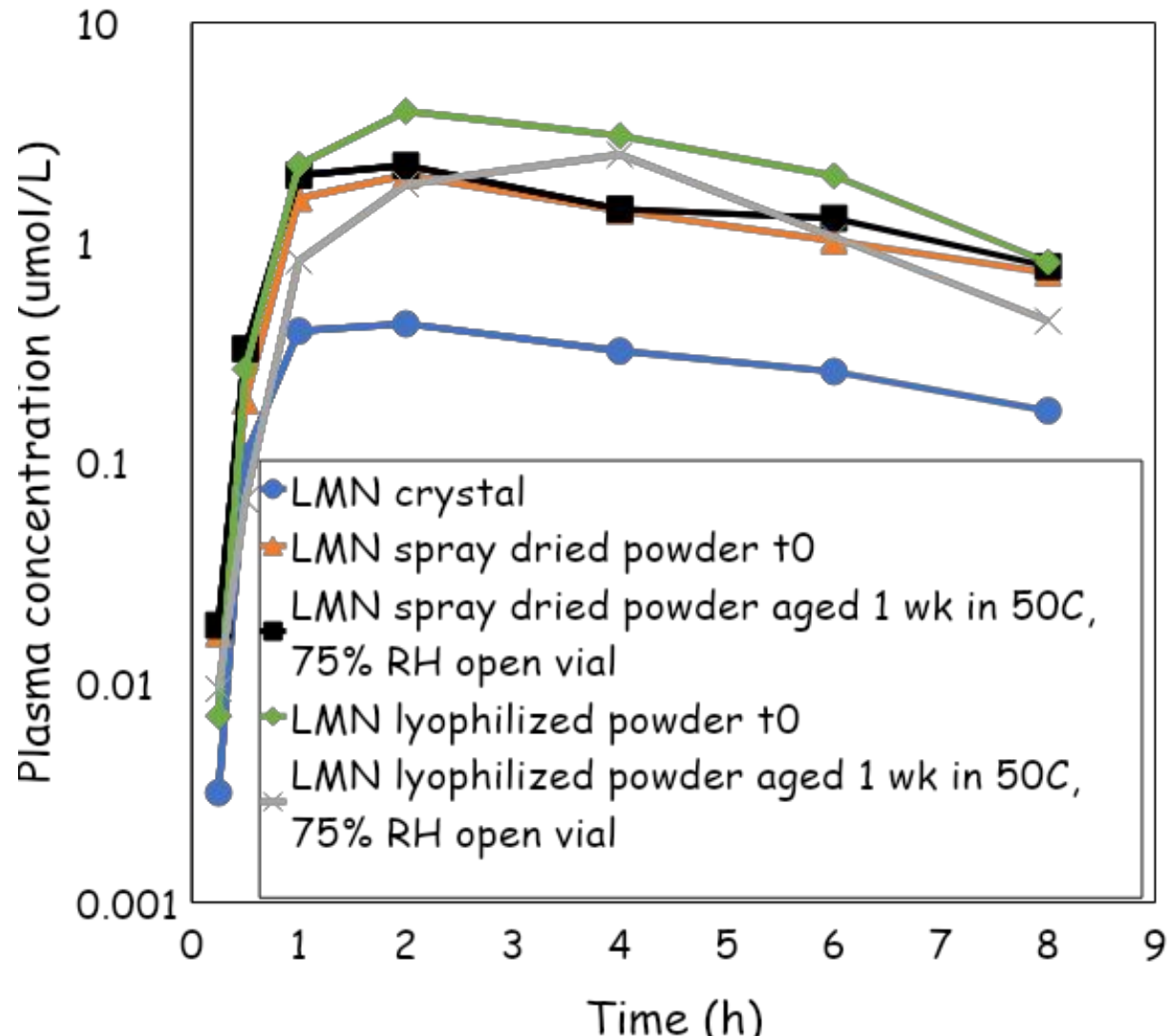
- 4 week stability under accelerated aging conditions (50C, 75% RH, open vial)
- Similar release kinetics in fasted or fed state media (no food effect)



# Enhanced bioavailability of LMN in animal study

*LMN NP powder samples **increased the bioavailability of the LMN 4.2X** compared to the crystalline drug*

LMN crystal powder	2.29
LMN spray dried powder t=0	9.74
LMN spray dried powder 1 wk	11
LMN lyophilized powder t=0	18.3
LMN lyophilized powder 1 wk	10.6



# Encapsulation by ion pair complexation

## Cinanzarine

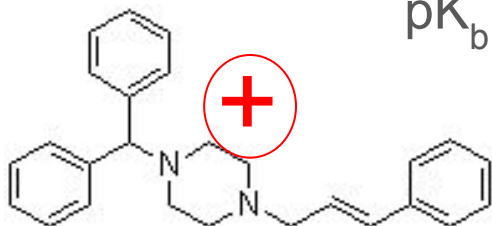
(antihistamine, weak base)

LogP

5.3

pK<sub>b</sub>

7.5, 1.95



- Individual cmds can not form stable NPs
- Complex eliminates polarity of charge groups

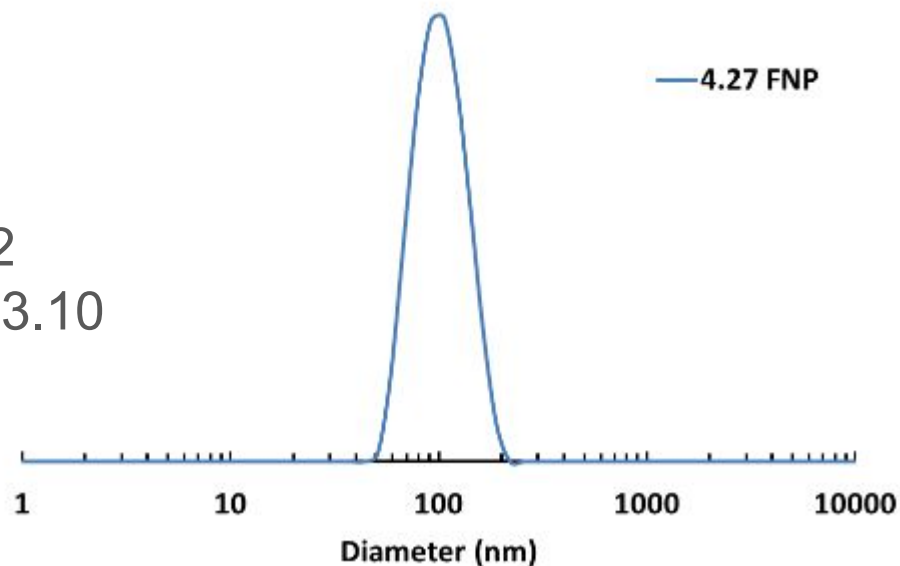
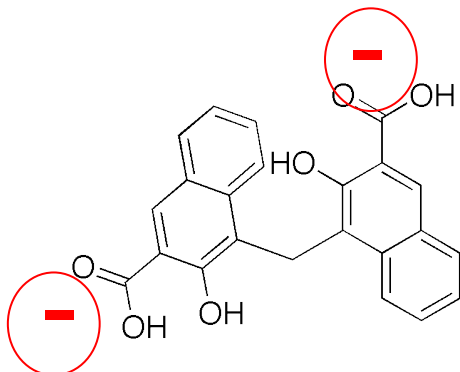
Pamoic acid (FDA approved salt)

LogP

5.52

pK<sub>a</sub>

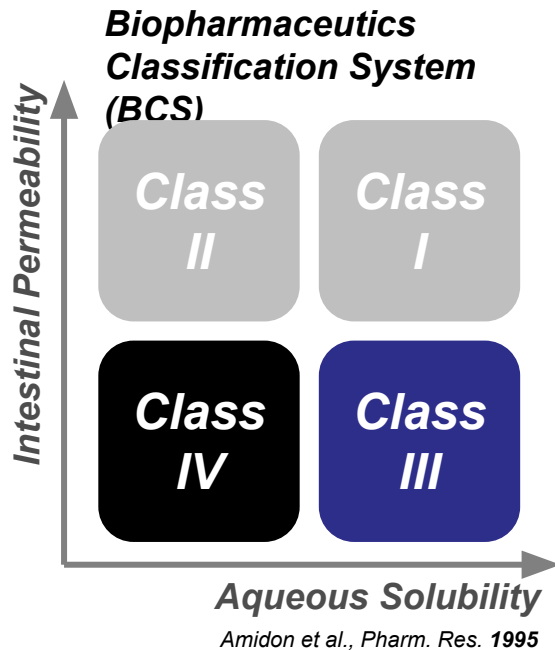
2.51 3.10



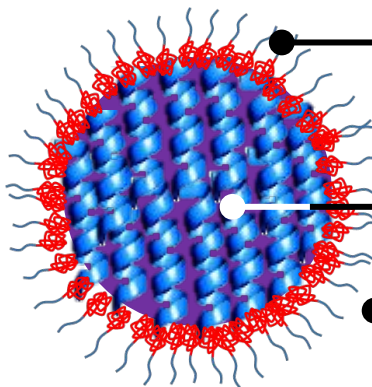
Pinkerton, Grandeury<sup>‡</sup>, Fisch<sup>‡</sup>, Jörg Brozio<sup>‡</sup>, Bernd U. Riebesehl et al., Mol Pharm (2012)

# Peptide nanoparticles by ion pairing: BMS-PCI

*Nanoencapsulation can help address solubility and permeability limitations to oral peptide delivery*



*Solubility and GI membrane permeability can vary widely with peptide architecture, charge, and functional modification*



-PEG brush facilitates muco-diffusion in GI tract

-Targeting ligands

Disordered core can enhance solubility

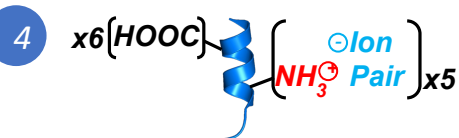
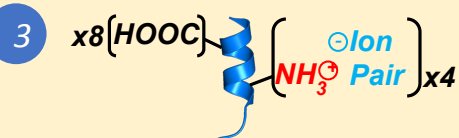
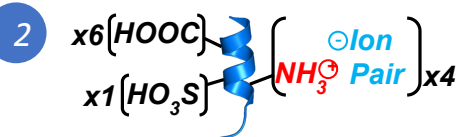
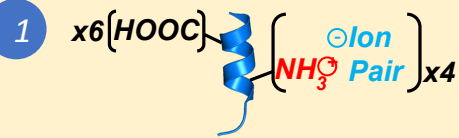
Tune ion pairing and stabilizer shell to modulate release kinetics

0.1% bioavailability

- insolubility
- too polar (soluble), membrane impermeable

# Peptide nanoparticles by ion pairing: BMS-PCI

Cyclic peptides synthesized by BMS  Bristol Myers Squibb

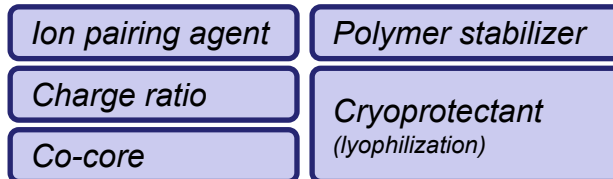


MW 2500-3500  
Da

Across four peptides variations in:

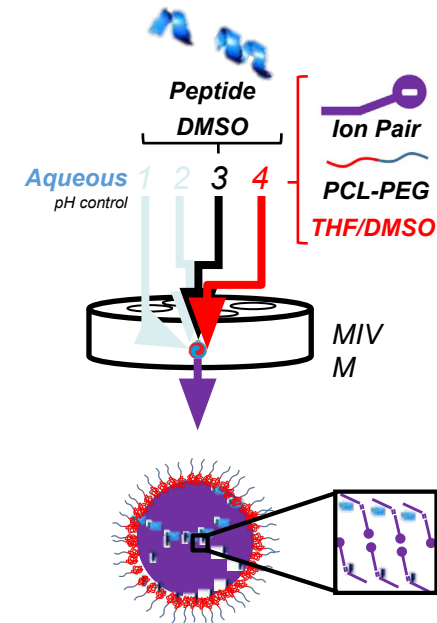


Parameters explored in FNP formulation:



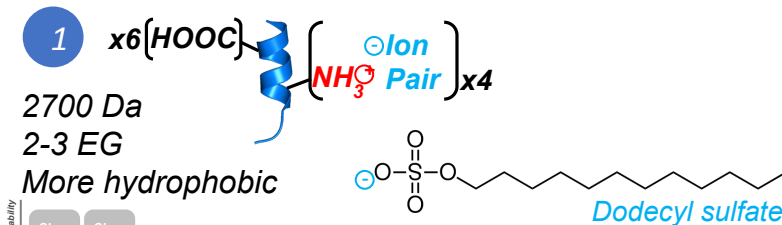
**Multi-Inlet Vortex Mixer (MIVM)**

Increased compositional and flowrate flexibility



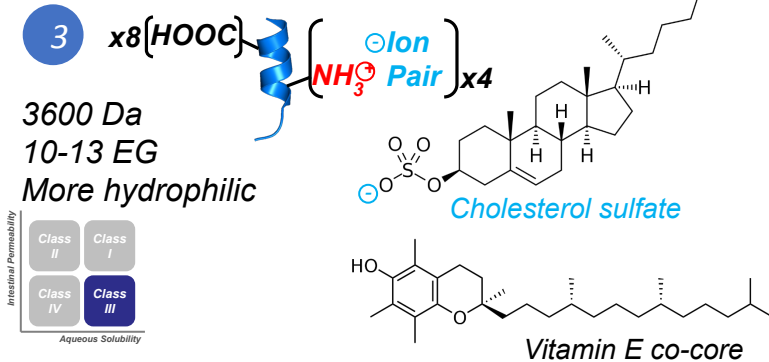
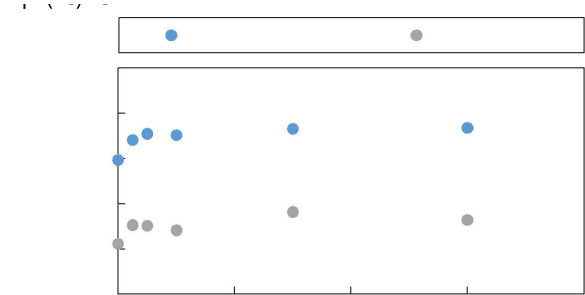
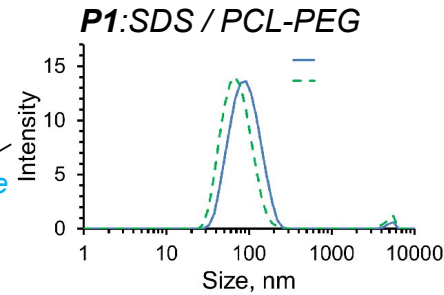
# Peptide nanoparticles by ion pairing: BMS-PCI

*Different formulation strategies required for more hydrophobic vs more hydrophilic peptides*



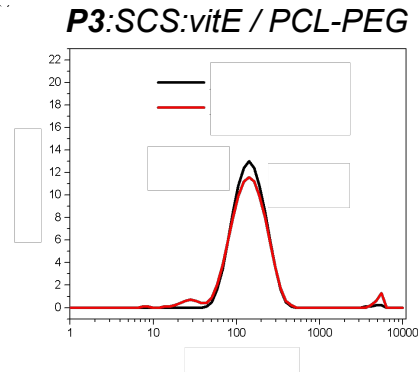
Class II	Class I
Class IV	Class III

Aqueous Solubility



Class II	Class I
Class IV	Class III

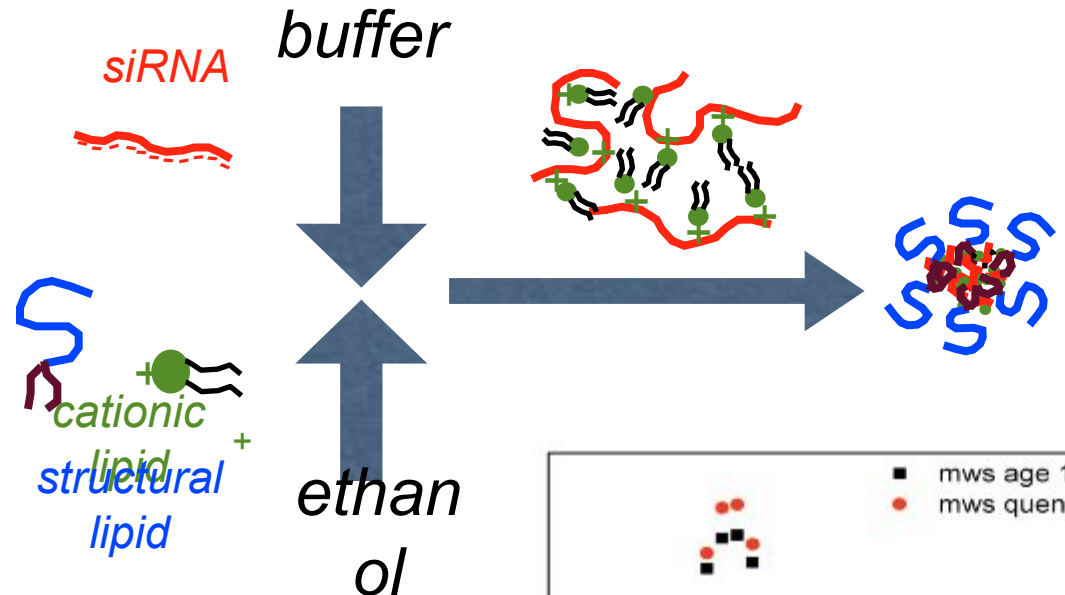
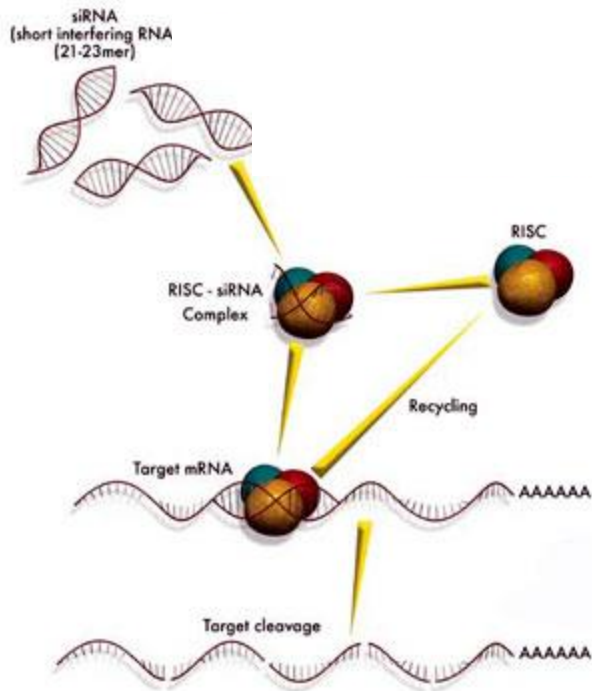
Aqueous Solubility



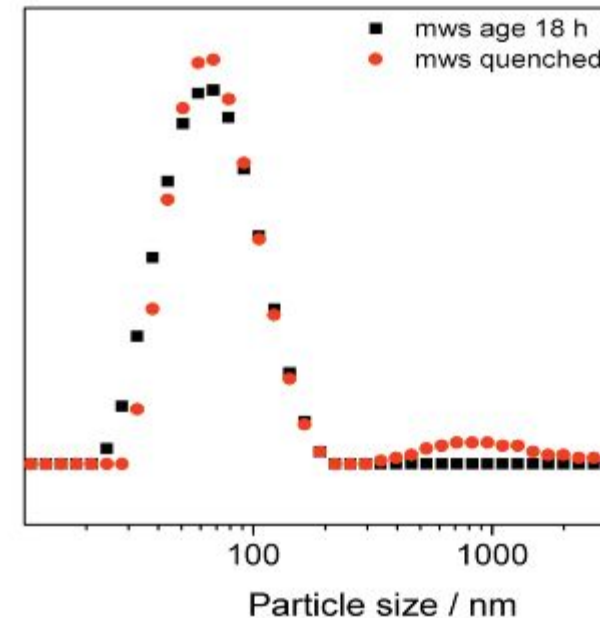
- *More hydrophobic peptide is directly ion paired with SLS*
- *More hydrophilic requires capture in a hydrophobic matrix*

# siRNA or mRNA Lipid Nanoparticles (Merck)

- *siRNA complex cleaves mRNA and stops protein expression*
- *Problem is delivery*



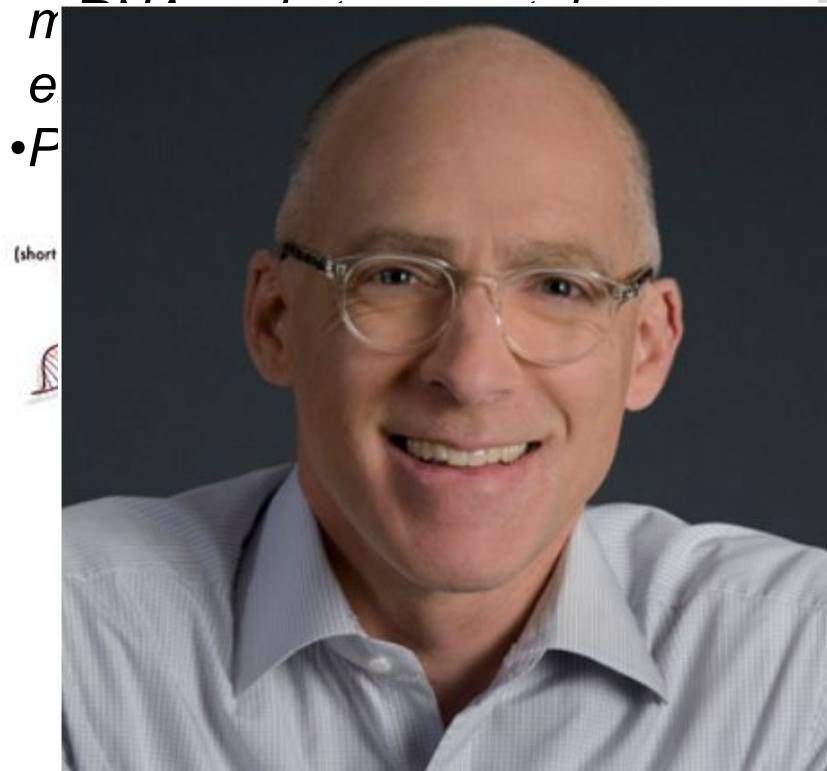
- *Successful prep of 100 nm PEG protected siRNA*
- *Stable and transfect efficiently*





# RNA Encapsulation

- siRNA complex cleaves



*Paul Burke*  
Merck



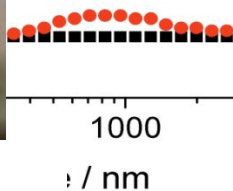
*Marian Gindy*  
Merck



*Varun Kumar*



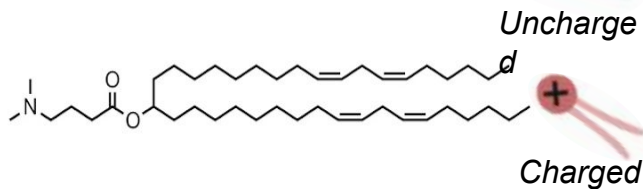
■ mws age 18 h  
● mws quenched



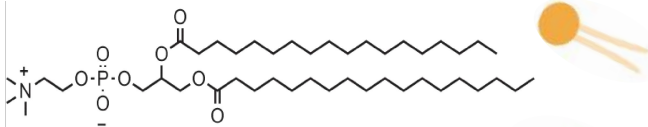
# mRNA and DNA Lipid nanoparticles (LNPs)

## LNP Formulation

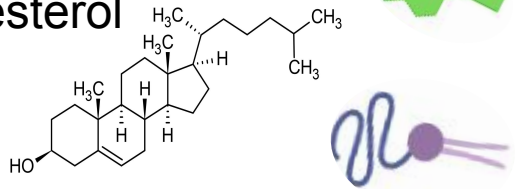
Ionizable lipid  
(Dlin-MC3-DMA)



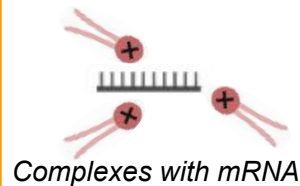
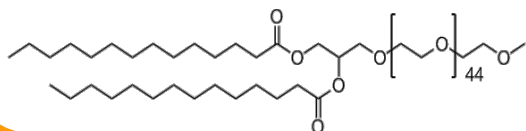
Zwitterion lipid (DSPC)



Cholesterol



Stabilizing lipid (DMG-PEG)



Complexes with mRNA

Stabilizes Structure

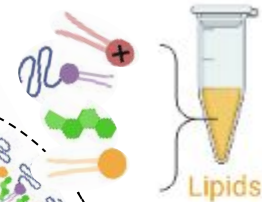
Provides Membrane Integrity & Rigidity

Prevents Aggregation

## Co-loading

Ethanol Solution

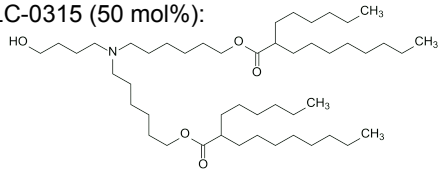
Aqueous Buffer Solution



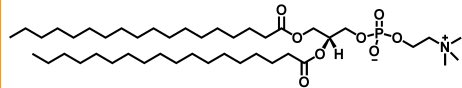
# Formulation and mRNA/DNA LNP production

## Formulation

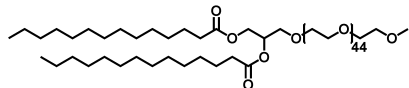
ALC-0315 (50 mol%):



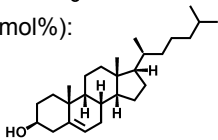
DSPC (10 mol%):



DMG-PEG<sub>2000</sub> (1.5 mol%):



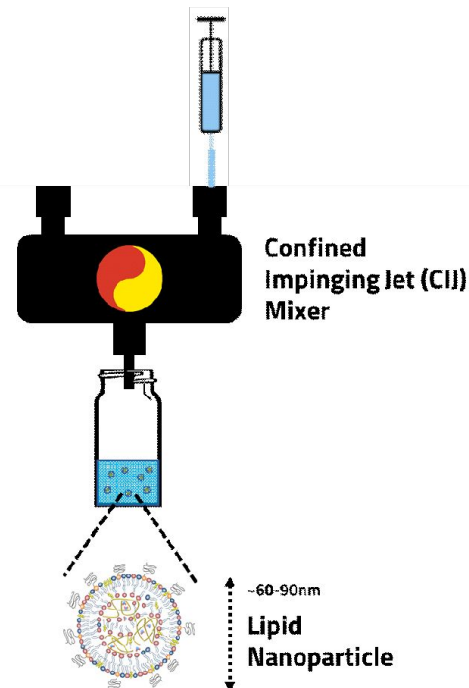
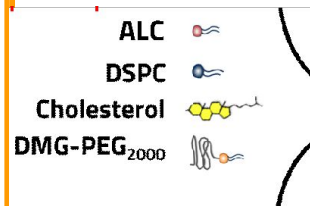
Cholesterol (38.5 mol%):



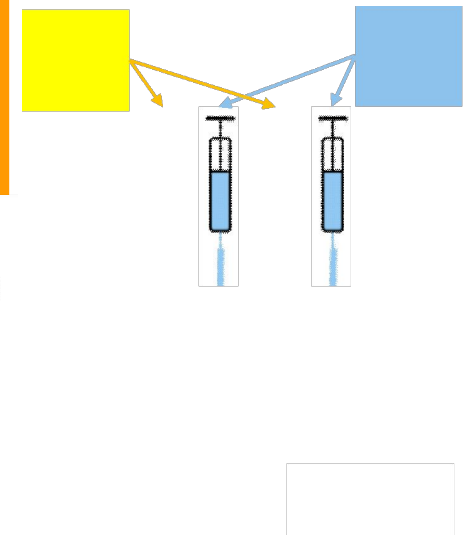
N/P 6 yeast RNA

10% EtOH

## CIJ setup



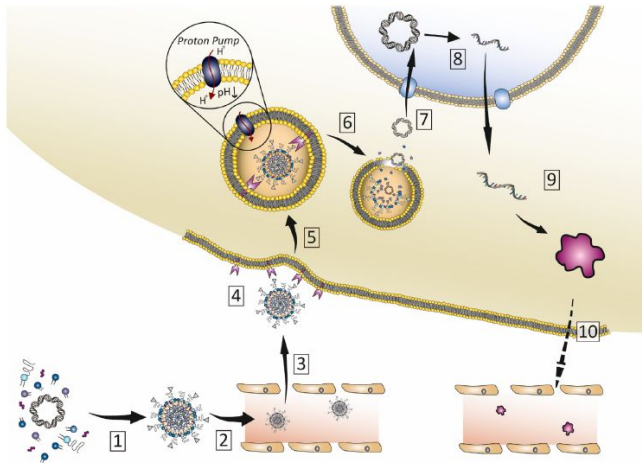
## MIVM setup



# DNA LNPs: Challenges and Opportunities

## Challenges:

- DNA stiffer than mRNA, more difficult to collapse
- Requires delivery to the nucleus



## Opportunities:

- FNP, iFNP targeting
- Can encapsulate larger DNA than AAVs

Buck, et al., *ACS Nano* 13, no. 4 (2019): 3754-3782.

## *Endosomal escape: Genentech - PCI*

**Solvent stream (Ethanol)**

DOPE

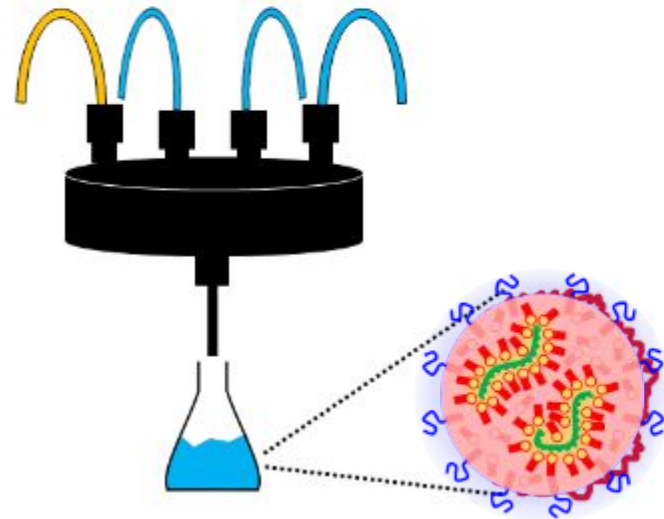
Dlin-KC2-DMA

**Stabilizer: PEG-DMG vs PEG-PCL**

**Anti-solvent stream (H<sub>2</sub>O)**

Sodium Acetate

pDNA or mRNA



# Four Scales of CIJ & MIVM

## CIJ

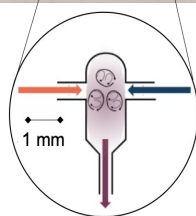
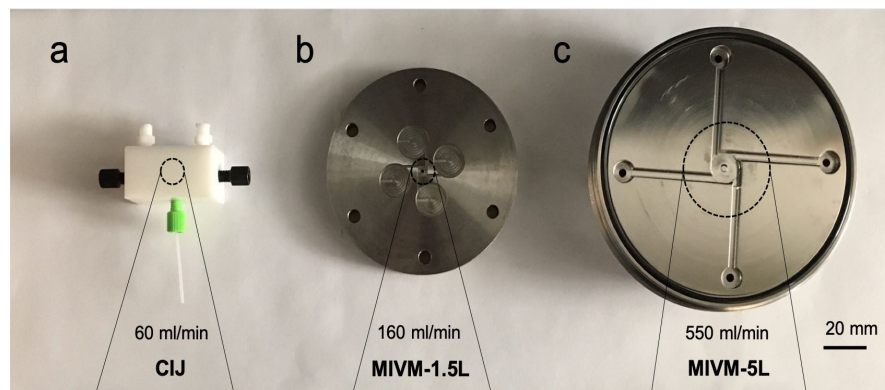
Confined Impinging  
Jet

## MIVM

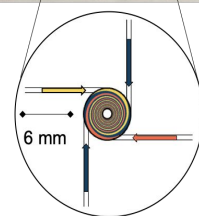
Multi Inlet  
Vortex Mixer

## Micro-MIVM

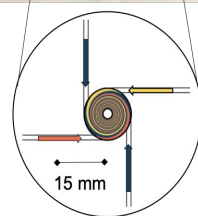
m-Multi Inlet  
Vortex Mixer



1 mL  
batch



1.5 L/min



5 L/min

Gates: 3700 tons/yr

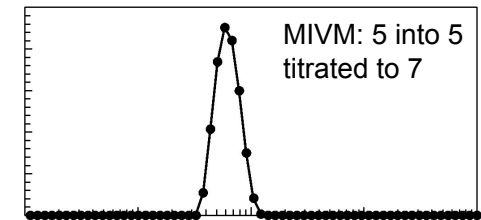
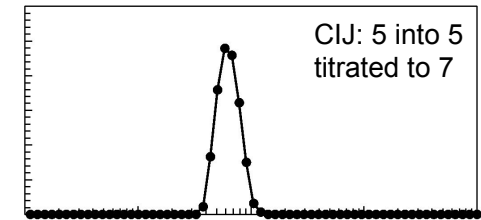
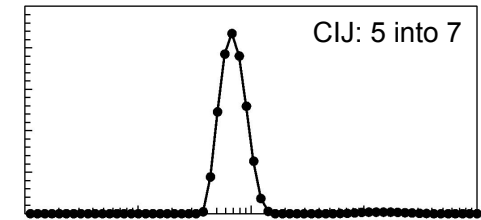
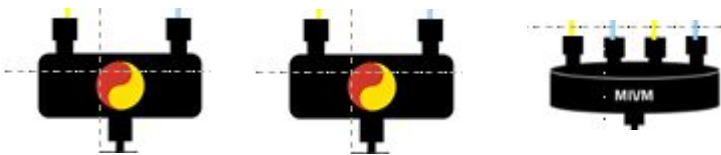
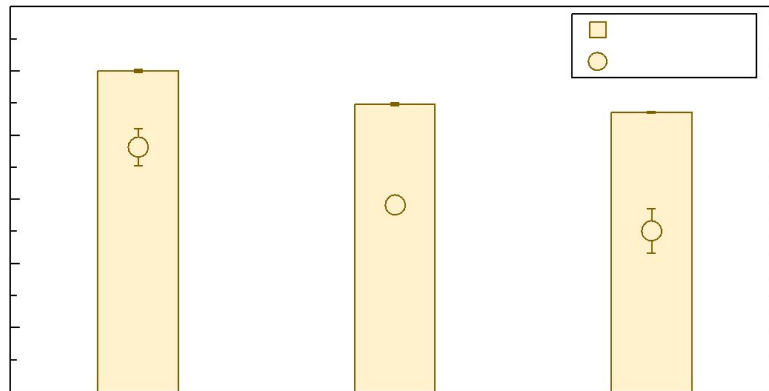


- 4 glass syringes: 2 ml
- 0.3-0.6 mg RNA (N/P=6)

Markwalter, et al JOVE **143** (2019), J Pharm Sci **107** (2018); Feng, J Trans Med submitted (2019)

# 50 nm DNA LNPs are produced via CIJ and MIVM

## No effect of mixer geometry



*LNP size is independent of pH  
shifting process: pH= 5  $\rightarrow$  pH 7*

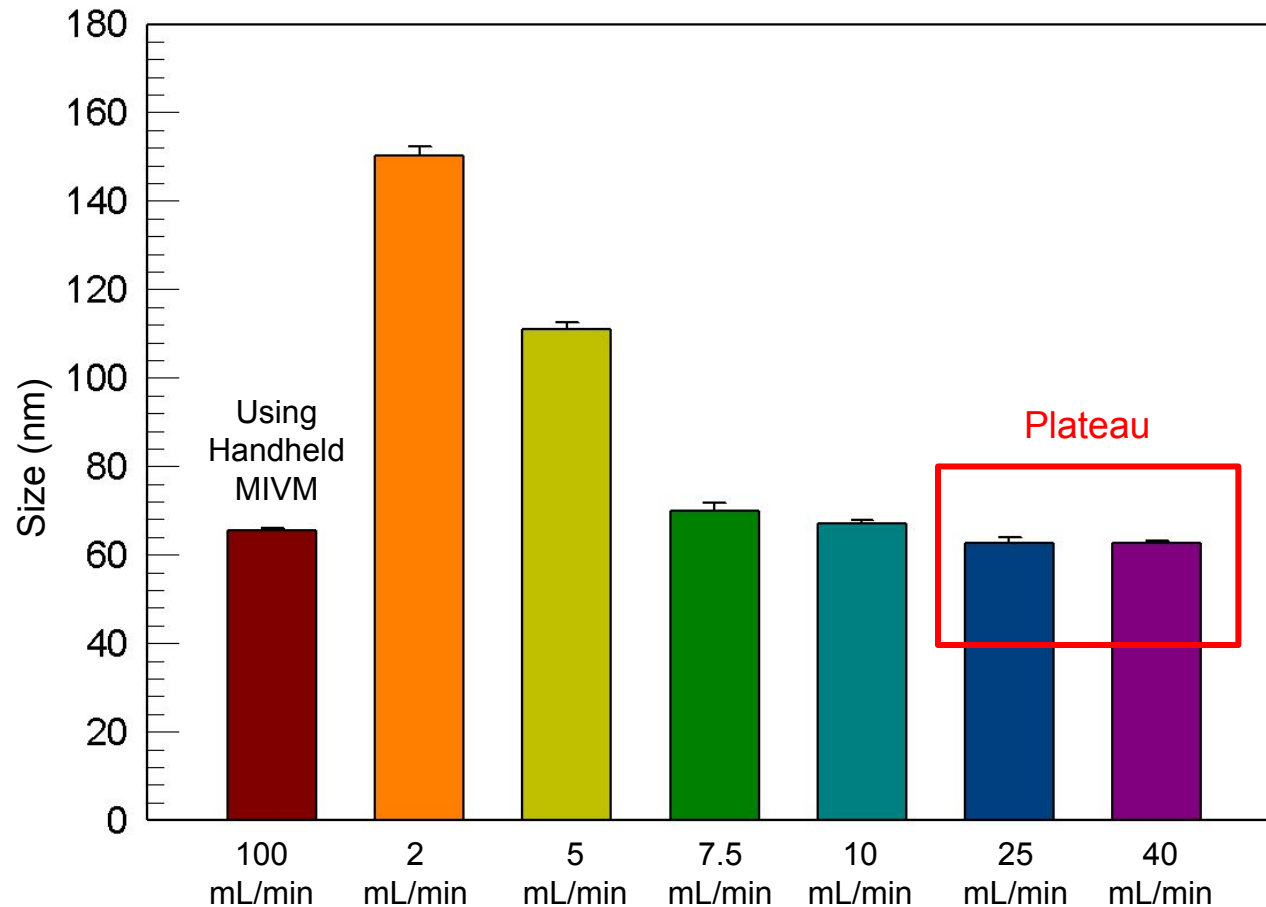


# Pump-based MIVM vs handheld MIVM

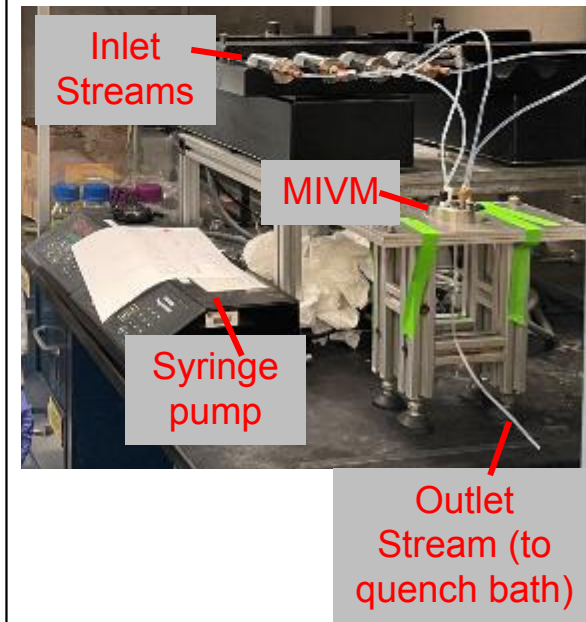
Before  
concentration

*DODMA lipid, mRNA (yeast) LNPs*

N/P ratio: 6



**MIVM setup**

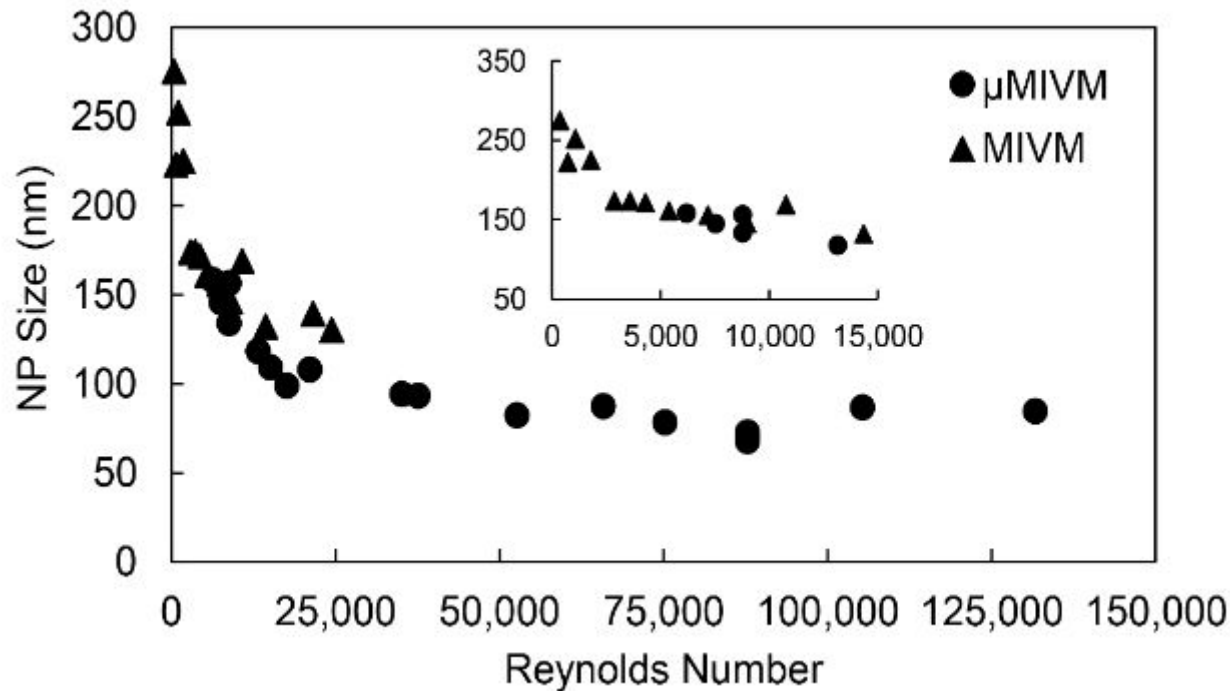


# Pump-based MIVM vs handheld MIVM

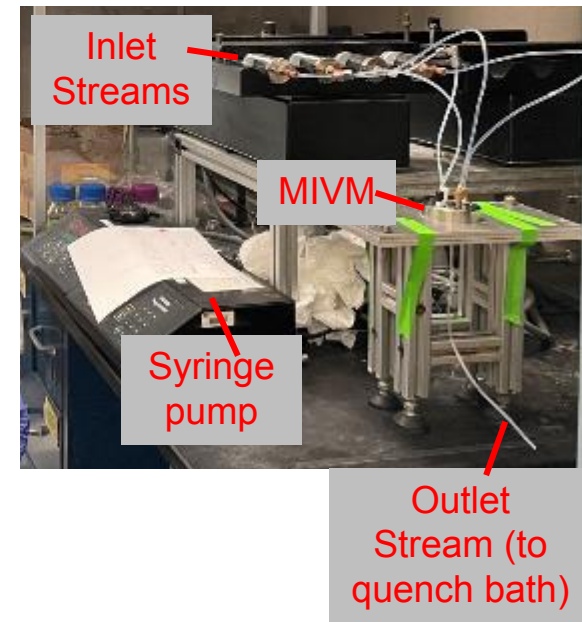
Before  
concentration

*DODMA lipid, mRNA (yeast) LNPs*

N/P ratio: 6



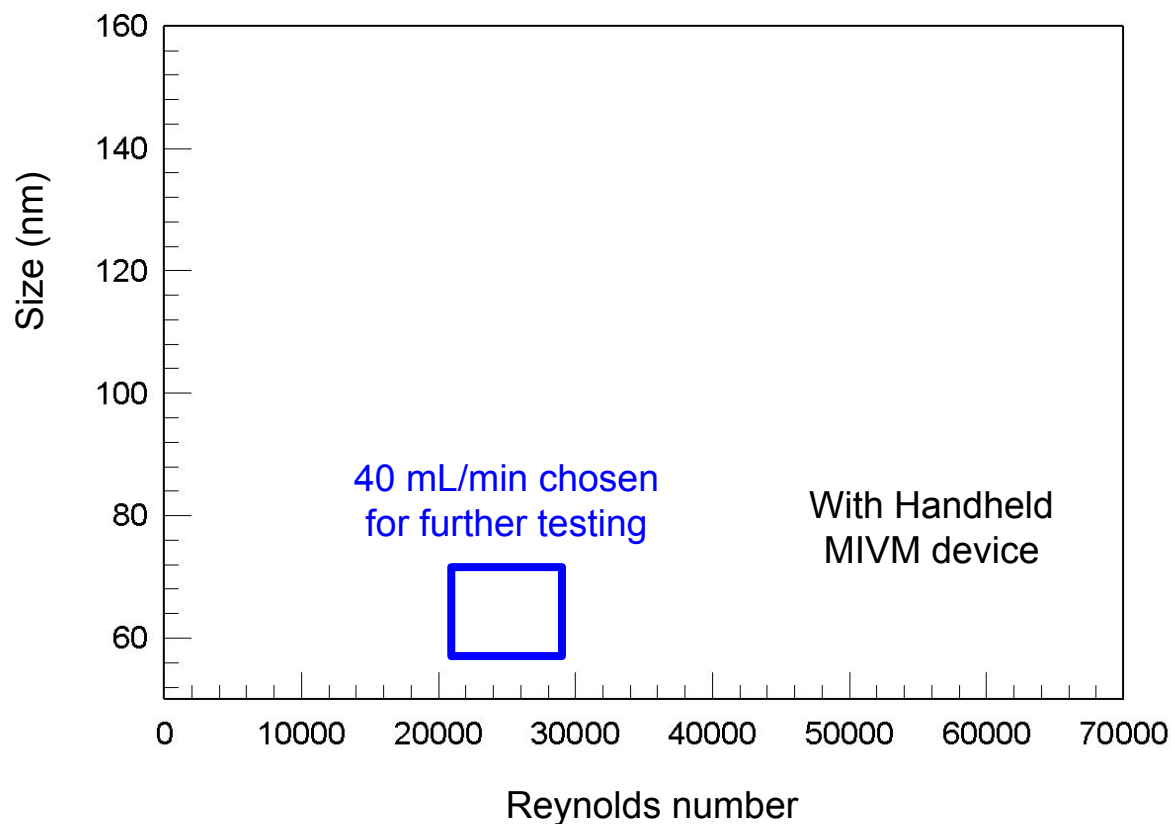
MIVM setup





## LNP RNA results

Understanding in terms of Size vs Reynolds number  
'DODMA lipid, yeast RNA



$$Re = \sum_{i=1,N} \frac{V_i}{\nu_i} D$$

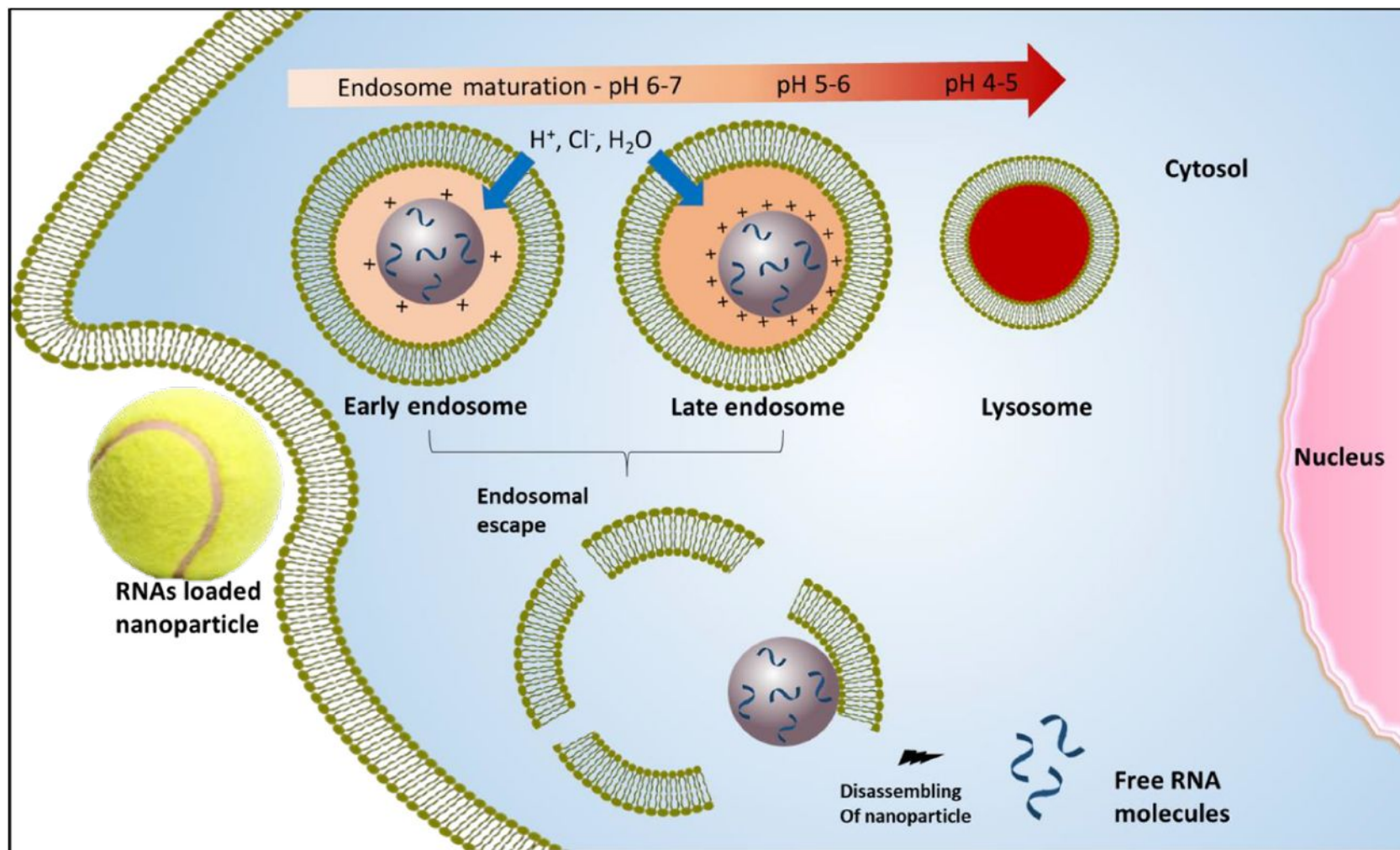
= Average inlet velocity of the *i*th stream

= Kinematic viscosity

= Chamber diameter

**Size of LNPs plateau at a critical *Re* of 15000!**

# Endosomal escape of COVID LNPs

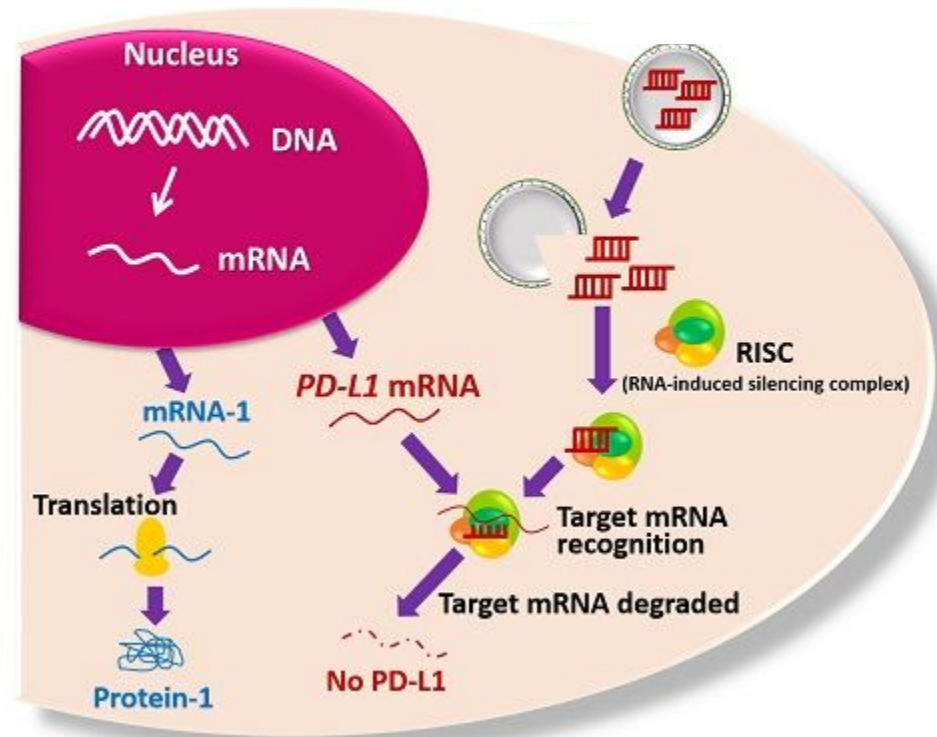


<https://doi.org/10.1016/j.tips.2021.03.002>

# Oligonucleotides

- **DNA** (deoxyribose nucleic acid): codes genetic information
- **siRNA** (silencing ribonucleic acid): stops mRNA synthesis
- **mRNA** (messenger RNA): synthesizes proteins

*Highly negatively charged, highly water soluble*



# Questions/Problems to Address: Targeting

## Targeting with more complex ligands: antibodies, nanobodies

- *Lipids are poorly anchored and large targeting ligands will pull lipids from LNPs*
- *Larger ligand-PEG-lipid can not be incorporated in LNPs by microfluidics*

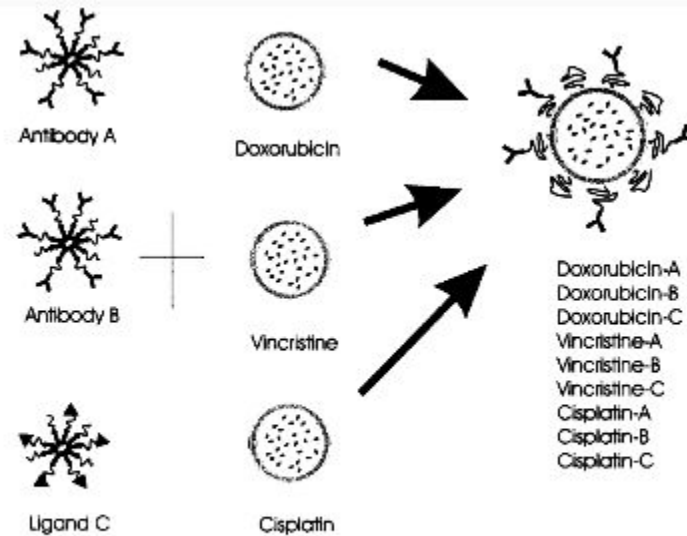
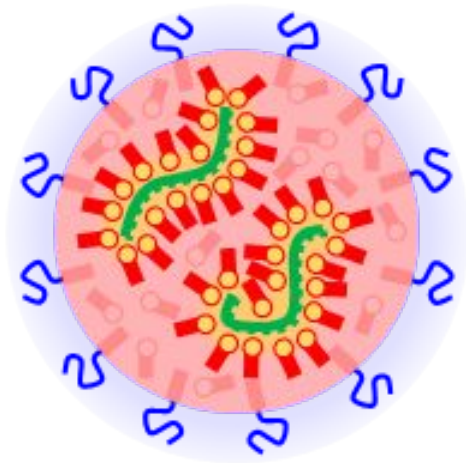


Fig. 1. Cartoon depicting the combinatorial approach to the formation of ligand-targeted liposomal anticancer drugs.

Ishida, T., D.L. Iden, and T.M. Allen, *A combinatorial approach to producing sterically stabilized (Stealth) immunoliposomal drugs*. FEBS letters, 1999. **460**(1): p. 129-133.

Parhiz, Hamideh, et al. "PECAM-1 directed re-targeting of exogenous mRNA providing two orders of magnitude enhancement of vascular delivery and expression in lungs independent of apolipoprotein E-mediated uptake." *Journal of controlled release* 291 (2018): 106-115.

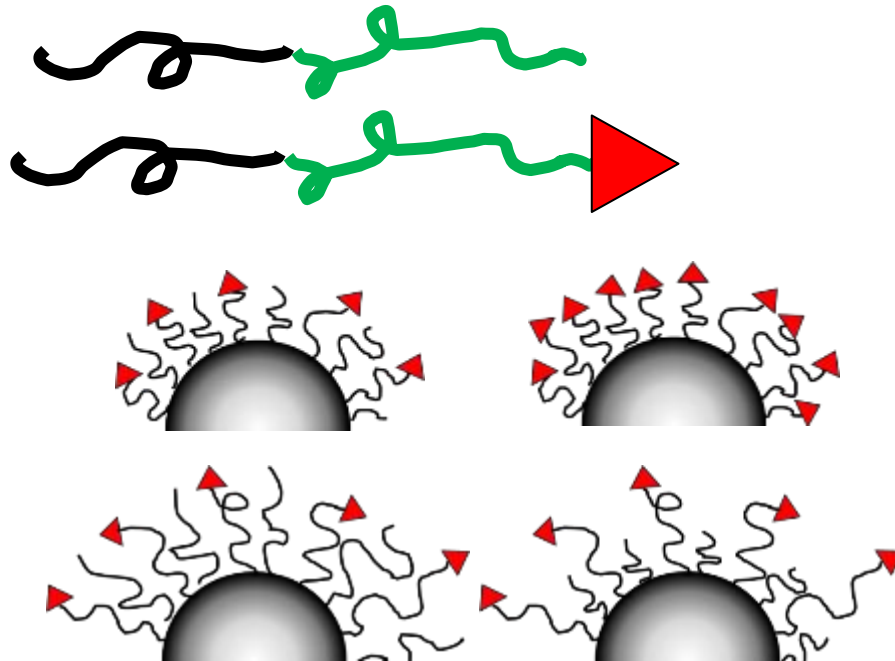
# Questions/Problems to Address: 4)Targeting

## **Targeting Summary:**

- 1) Targeting by changing LNP surface charge can bias deposition in the liver/lungs/spleen*
- 2) Adding cationic lipids to alter charge raises immunogenic problems*
- 3) Targeting using “high specificity ligands” (e.g. antibodies) will require a different platform than current LNP processes*

# Active targeting

- Conjugate targeting group to block copolymer
- Do hard chemistry and characterization on conjugate
- Quantitatively assemble targeted NP with control on % targeting groups
- Conjugate chemistry: click chemistry, maleimide, carbodiimide, carbamate



Small molecule:  
(mannose, folate, LHRH)



V domain



V<sub>H</sub>

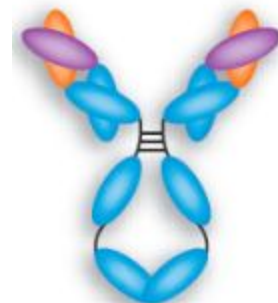


V<sub>K</sub>

scFv



IgG

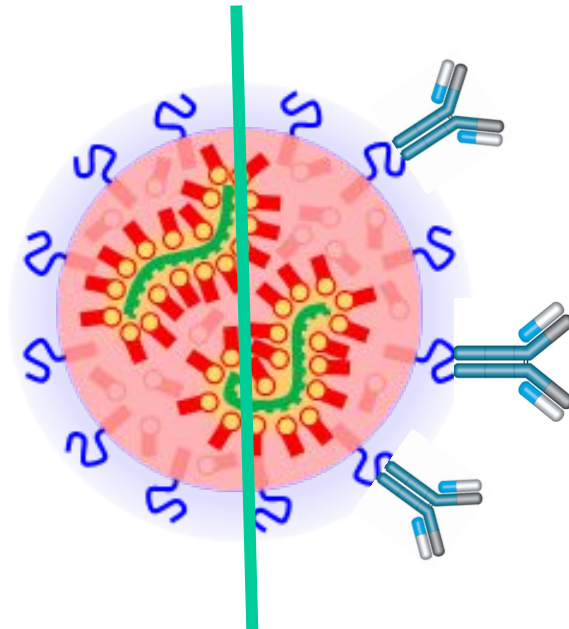




# Targeting mRNA and DNA LNPs

## Current LNPs

- Anchored by lipid (PEG-lipids)
- Meant to partition off in 30 min



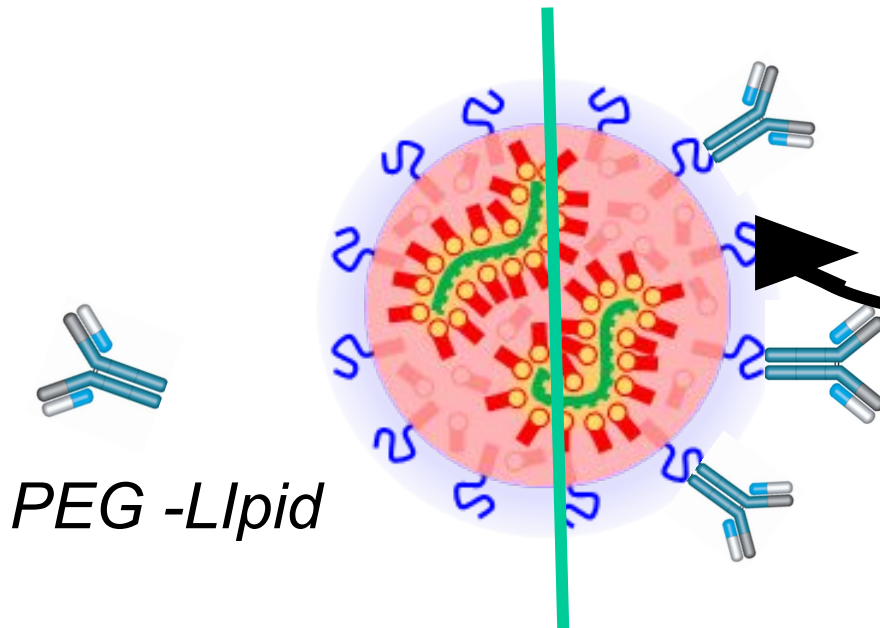
## Princeton NPs

- Anchored by block copolymer: PEG-PCL
- Irreversibly anchored
- Targeting antibody conjugated to PEG
- **Question:** does PEG layer prevent endosomal escape?

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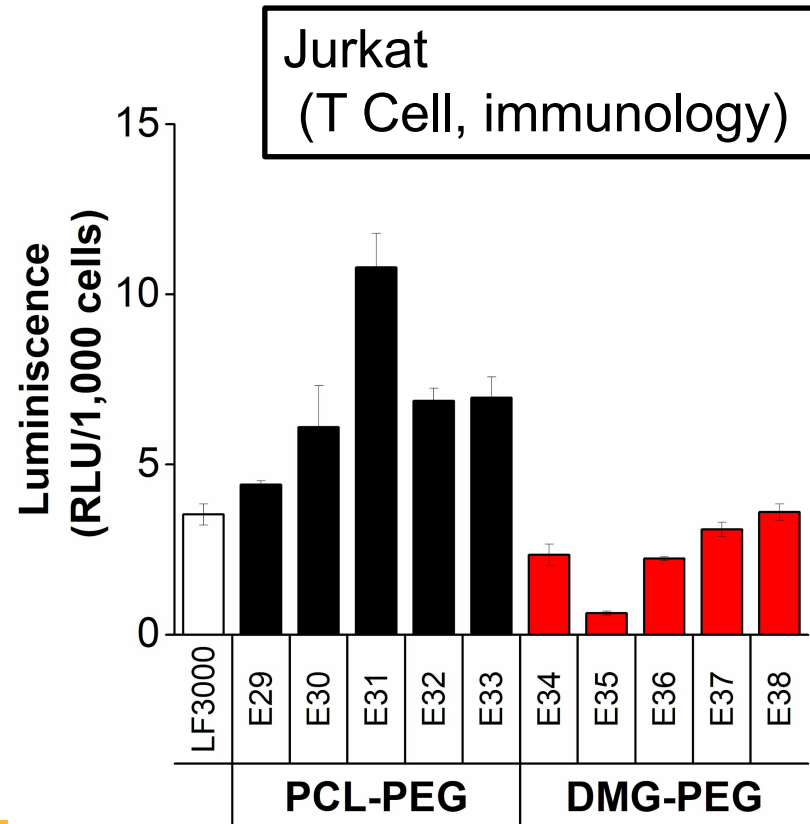
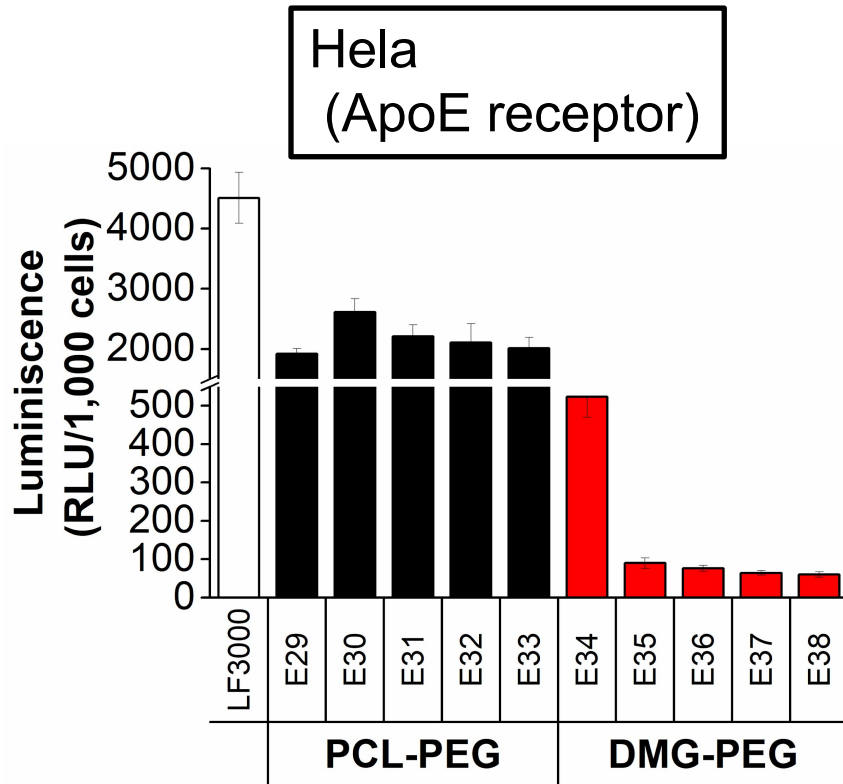
- Anchored by block copolymer: PEG-PCL
- Irreversibly anchored
- Targeting antibody conjugated to PEG
- **Question:** does irreversible PEG layer prevent endosomal escape?

PEG -PCL



# DNA LNPs by FNP: lipid vs PCL polymer anchoring

- *PEG-lipids are designed to partition off the LNP*
- *PEG-PCL (block copolymers) stay anchored, provide a basis for targeting*
- **Does anchored PEG prevent endosomal escape or transfection?**
  - **No! PCL-PEG DNA transfects better than lipid-PEGS**
  - **Similarly to Lipofectamine 3000**



# Outline

1. ***Nanoparticles by turbulent micromixing in confined impinging jet mixers (CIJ)***
  1. *Development of an idea: Flash NanoPrecipitation (FNP)*
2. ***Nanoparticle drug delivery***
  1. ***Oral:*** *increased bioavailability (Gates funding)*
  2. ***Parenteral:*** *Controlled release with conjugation*
  3. ***Parenteral:*** *Ion pairing for hydrophilic drugs (LNPs RNA, peptides, proteins)*
3. ***mRNA and DNA Lipid Nanoparticles: Targeting***

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3. ***Targeting***
4. ***Inverse FNP of biologics: NPs and Depot MCs***

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# “It takes a village”

