

# sustained drug release injectables

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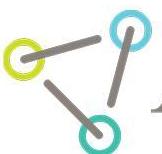
polymer design, formulation, and  
processing for success

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ashland.com

/ efficacy usability allure integrity profitability™



Ashland™  
always solving

# core strengths

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## tablet binding

Ashland produces binders for wet granulation, dry granulation, direct compression and roller compaction, as well as hot-melt extrusion.



## modified release

Our extensive product lines offer various degrees of both hydrophilicity and molecular weights, providing you with a host of options.



## tablet disintegration

Polyplasdone™ crospovidone provides rapid disintegration and dissolution of oral solid-dosage forms, even at low use levels.



## drug solubilization

High-quality excipients that improve the solubility of your API.



## film coatings

Fully formulated film-coating systems, easily dispersed and provides a range of functions to suit almost any tablet core.



## parenteral applications

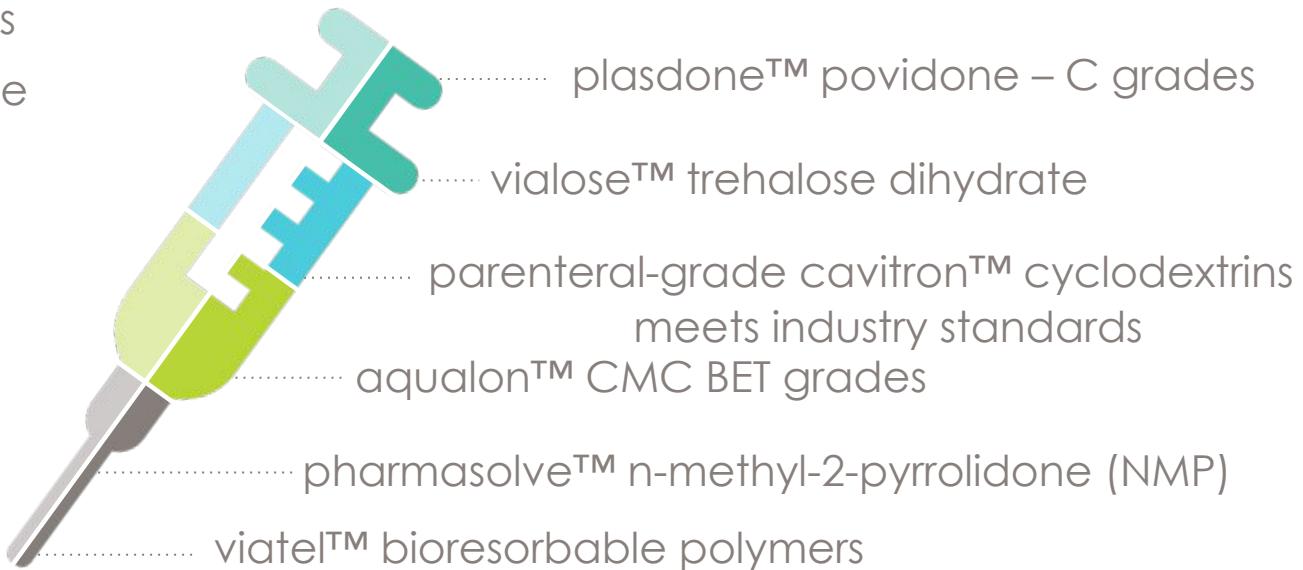
Ashland provides a suite of products that are be suitable for use in **parenteral, controlled release drug delivery systems**.

# excipients for parenteral use

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parenteral applications  
require excipients of the  
**highest quality**

Ashland's **high-purity**  
excipient portfolio



# outline

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## overview of drug delivery strategies using bioresorbable polymers (BRP's)

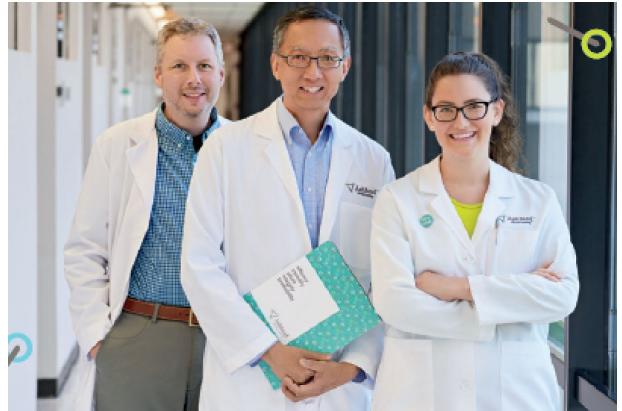
- purpose of bioresorbable polymers in drug delivery
- introduction to formulation formats
- commercial products

## controlling drug release via BRP chemistry

- detail natural polymer degradation pathway
- controlling formulation degradation by polymer selection

## formulation selection process & chemistry for extended drug release

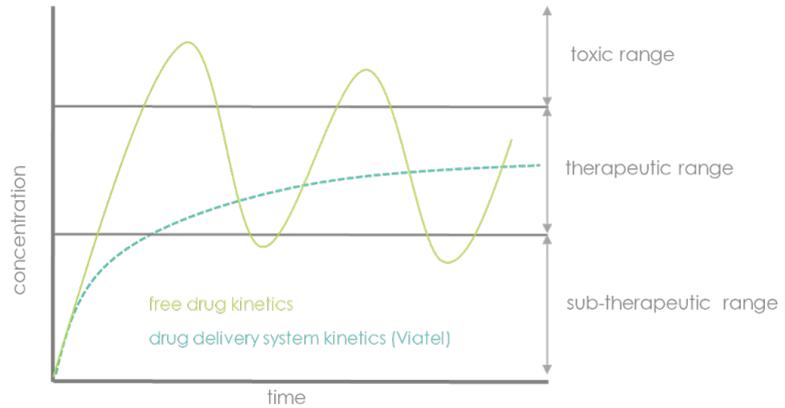
- choosing formulation process
- breakdown of multiple formulation options



# purpose of BRPs in pharma

## many drugs present

- toxicity, fast metabolism and excretion
- low uptake / PK variability after oral administration
- low concentrations in the desired location via oral routes



## advantages of injectable sustained release drug delivery

- tuneable (days – months) drug release
- decreased overall drug dosage / local delivery = reduced side effects
- therapeutic window
- simplify drug stability through digestive system and metabolic variance
- case dependent advantages (carriers, molecule types, other)

# viatel™ BRP product families

## for drug delivery

- poly D,L-lactide (PDLLA)
- poly D,L-lactide-co-glycolide (PLGA)
- poly caprolactone (PCL)
- poly D,L-lactide-co-caprolactone (PLCL)

## all products have high purity

- no residual solvents
- low residual tin

## other

- 70+ in-stock offerings
- custom polymers available

in-stock offerings			
monomer composition	co-monomer ratio(s)	end-cap	inherent viscosity ranges (dL/g)
poly(D,L-lactide) (PDLLA)	--	acid ester	0.1 - 1.4 (multiple grades)
poly(D,L-lactide-co-glycolide) (PLGA)	50:50 55:45 65:35 75:25 85:15	acid ester	0.1 - 1.4 (multiple grades)
polycaprolactone (PCL)	--	ester	1.0 - 2.0 (multiple grades)
poly(L-lactide-co-caprolactone) (PLCL)	60:40 70:30 80:20 90:10	ester	1.0-1.4

# PLGA parenteral products history

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1930s-60s

early patents and publications

1971 Dexon: first synthetic bioabsorbable suture (not drug delivery)

1973 DuPont: first lactide / glycolide drug delivery patent

1986 Decapeptyl\*: first injectable extended-release microparticle product

1989 Zoladex\*: first implantable extended-release implant product

2001 Atridox\*: first local delivery product

2002 Eligard\*: first injectable extended-release lactide/glycolide in-situ forming product

2006 SmartShotB12: first injectable microparticle for animals

2007 Genexol\* PM: first nanoparticle

2009 Ozurdex\*: first product for ocular delivery

2011 Propel\*: first drug-eluting device

2011 Revalor\*: XS First implantable for animals

2016 Reseligo: first generic implantable

2016 Absorb GT1\*: first bioabsorbable drug-eluting cardiovascular stent

2017 Zilretta\*: first micro-particle product for intra-articular delivery (knee)

# PLGA-based sustained release formulations

## in situ forming systems

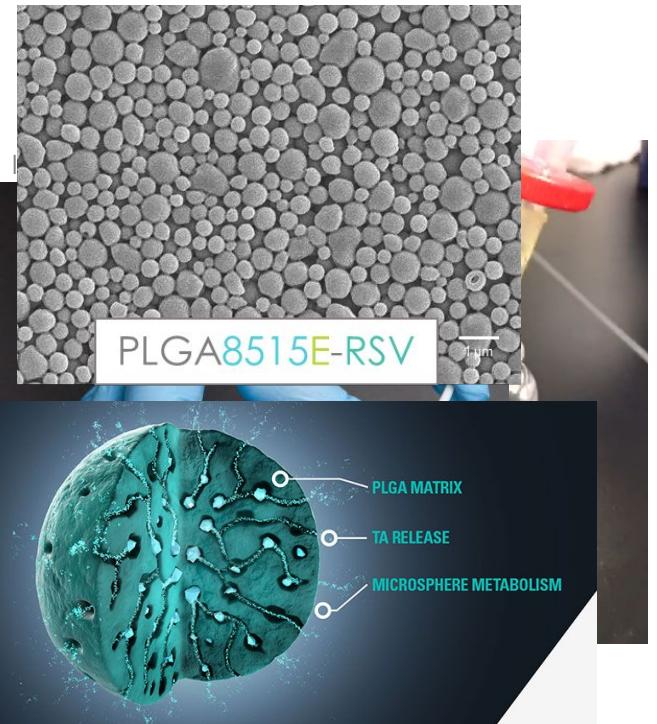
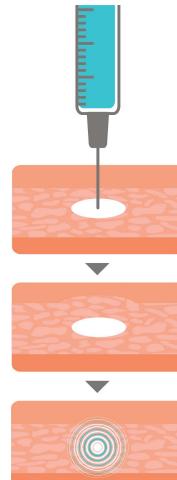
- API + PLGA + solvent
- formed in vivo, simplified process and costs,
- administered through injection, larger burst effect, implant shape variance

## solid implants

- API + PLGA
- no organic solvents, good stability, lower burst effect
- extrusion (thermal deg.), administered through surgery or injection

## particle technologies

- API + PLGA + diluent
- microspheres, nanoparticles
- smaller needles, tuneable profiles
- organic solvents, particle stability, complexity (aggregation)



# commercial product examples

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- **in situ forming depot**

e.g., Eligard\*—leuprolide acetate  
(sub cutaneous injection; 1, 3, 4 or 6 monthly)



- **microsphere technologies**

e.g., Bydureon\*—exenatide depot  
(weekly self-administered subcutaneous injection)



- **solid implants**

e.g., Ozurdex\*—intravitreal dexamethasone implant (injection)



# product examples

brand name	indication	company	drug substance	API Size (Da)	dose (mg)	months
Eligard*	Prostate cancer	Sanofi-Aventis	Leuprolide acetate	1260 (peptide)	7.5 – 45	1, 3, 6
Sublocade*	Opioid dependency	Indivior	Buprenorphine	467.64 (SMD)	100, 300	1
Longrange*	Parasite treatment	Merial Limited	Eprinomectin	914 (SMD)	50	5
Bydureon*	Diabetes (II)	AstraZeneca	Exenatide	4187 (peptide)	2	0.25
Sandostatin* LAR	Acromegaly / flushing / cancer-induced diarrhea	Novartis	Octreotide acetate	1079 (peptide)	10 – 30	1
Decapeptyl* SR	Prostate cancer	Ipsen / Ferring	Triptorelin pamoate	1700 (peptide)	4 – 28	1, 3, 6
Scenesse*	Erythropoietic protoporphyrin (light intolerance)	Clinuvel	Afamelanotide	1707 (peptide)	16	2
Zoladex* 1 / 3 month	Prostate / breast cancer	AstraZeneca	Goserelin Acetate	1269 (peptide)	3.6 – 10.8	1, 3
Revalor*	Growth promotion (animal)	Intervet / Merck Animal Health	Trenbolone / estradiol	270 / 272 (SMD)	140 / 14	6

# needle delivery format

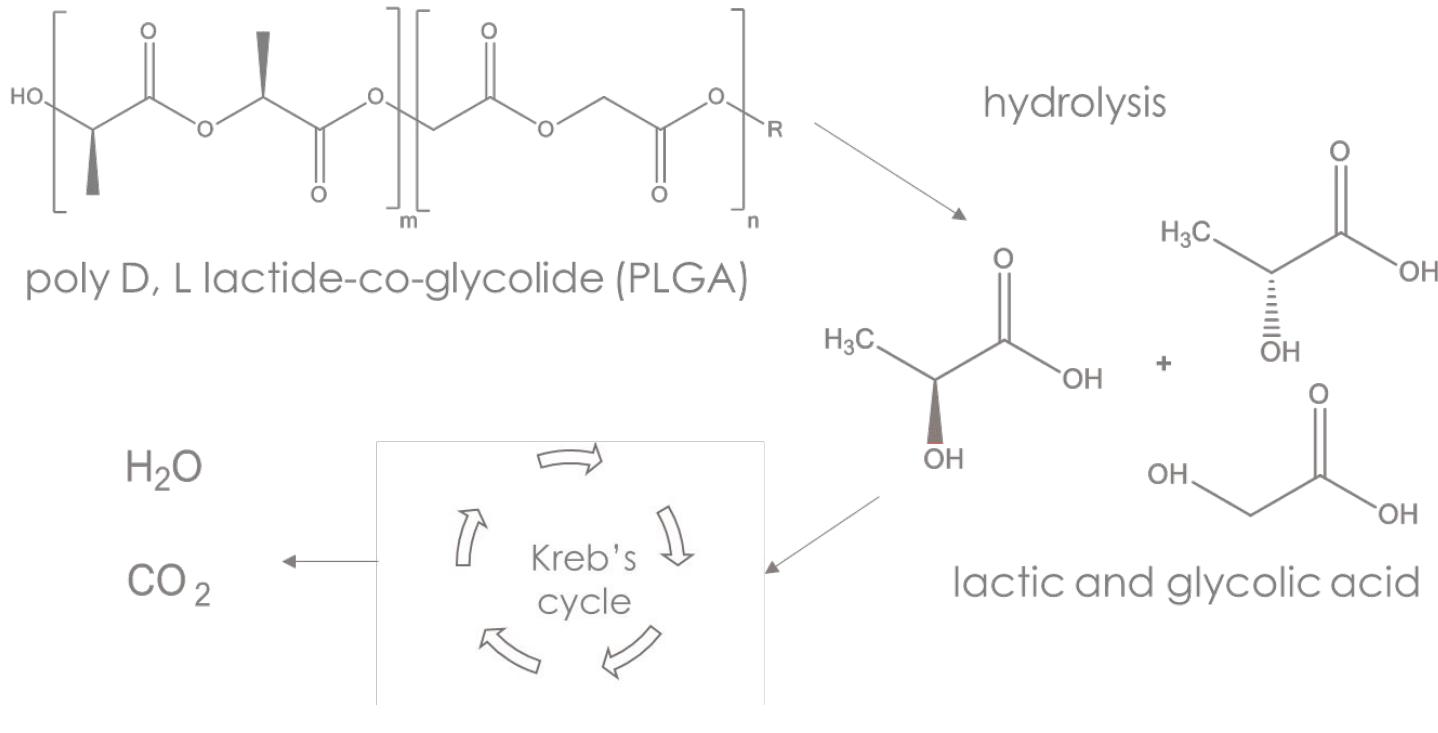
product	formulation type	needle size
Fensolvi*	in situ gel	18 G
Sublocade*	in situ gel	19 G
Perseris*	in situ gel	18 G
Lupron* Depot PED	microsphere	23 G
Bydureon*	microsphere	23 G
Decapeptyl* SR 11.25 mg	microsphere	20 G
Ozurdex*	implant	22 G
Zoladex*	implant	3.6 mg dosage: 16 G 10.8 mg dosage: 14 G





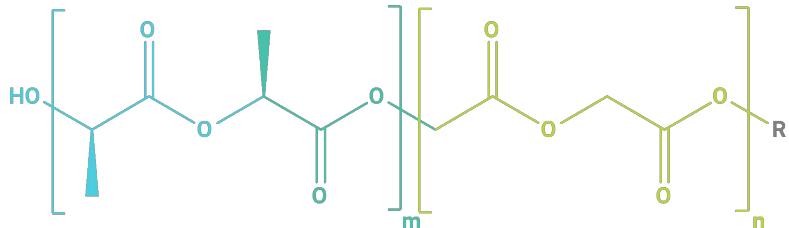
controlling drug release via  
BRP chemistry

# what happens to PLGA in the body?



# BRP chemistry & structure

## poly D, L lactide-co-glycolide (PLGA)



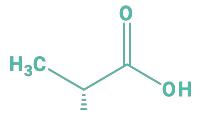
## end group options

R = acid

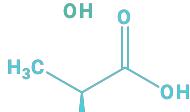
R = ester

R = other

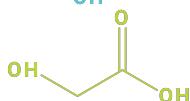
## monomer options



= D-lactic acid



= L-lactic acid



= glycolic acid

## chemical characteristics

inherent viscosity or  
molecular weight and  
polydispersity:

no. of repeating  $m$  &  $n$  units  
and chain length variance

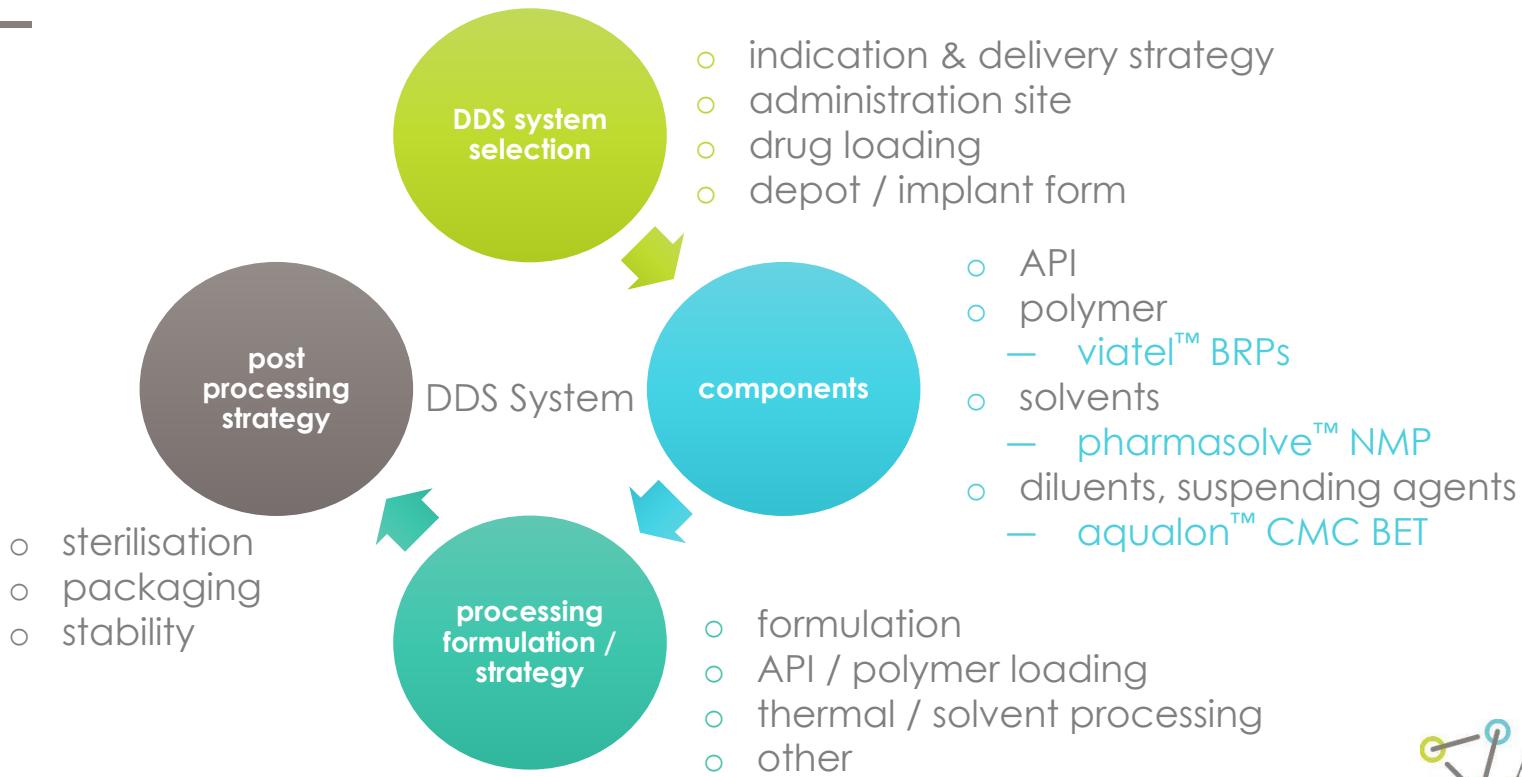
# theoretical polymer influence on release

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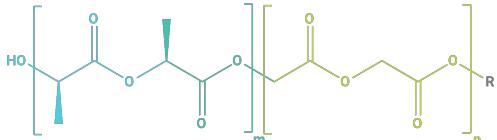
polymer characteristic	option & effect
molecular weight / inherent viscosity	<ul style="list-style-type: none"><li>higher Mw / inherent viscosity = increased release duration</li></ul>
lactide : glycolide content	<ul style="list-style-type: none"><li>increased lactide content = increased hydrophobicity = increased release duration</li></ul>
polymer end-cap	<ul style="list-style-type: none"><li>acid = hydrophilic</li><li>ester = hydrophobic = increased release duration</li></ul>

# drug delivery system – we can help

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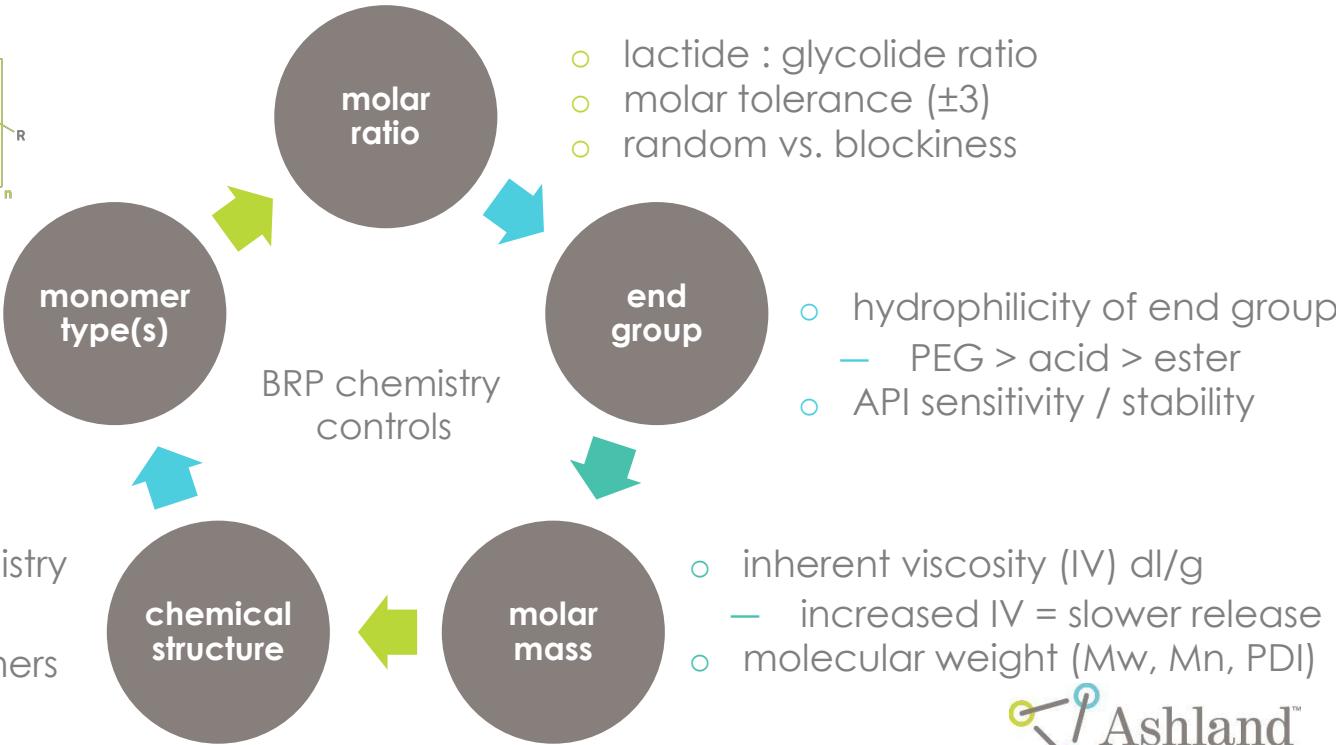


# polymer functions to control release



- monomer inclusion
  - D,L lactide
  - glycolide
  - L lactide
  - $\epsilon$ -caprolactone

- incorporate other chemistry
  - e.g., glucose
  - star / dendritic polymers
  - new polymers



# put the theory to the test

## Eligard® (leuprolide acetate)

- long-acting polymer
  - 82.5 mg poly D,L lactide-co-glycolide 50:50 A
- biocompatible solvent
  - 160 mg N-methyl-2-pyrrolidone (NMP)
- active pharmaceutical ingredient



long-acting variations			
month(s)	leuprolide acetate (mg)	polymer	solvent
1	7.5	PLGA 50:50 A	NMP
3	22.5	PLGA 75:25 E	NMP
6	45	PLGA 85:15 E	NMP

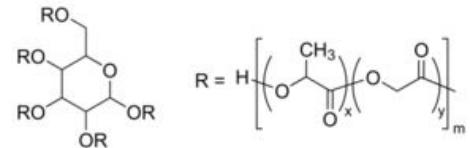
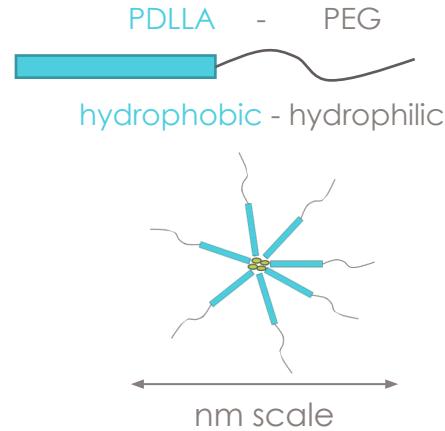
# other polymer structures

## chain end-group

- PEG addition – stability, faster water uptake, and release
- tune degradation (PCL-PEG example)
- amphipathic structure (e.g. Genexol\*)

## monomer composition & polymer structures

- caprolactone, lactide, glycolide
- structure: di- and tri-block structures, glucose-star, dendritic copolymers
- varied release profiles, stability, physicochemical properties





formulation strategies & optimization

# formulation options

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active pharmaceutical  
ingredient



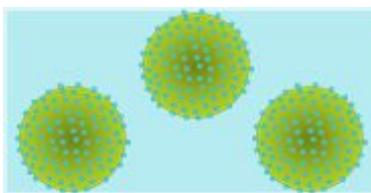
bioresorbable polymer



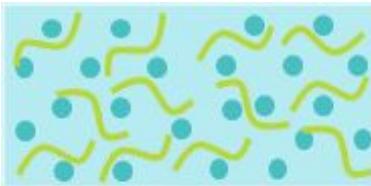
solid implant



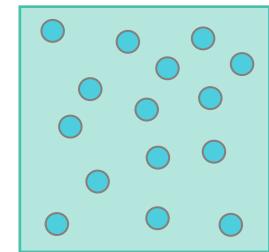
particles



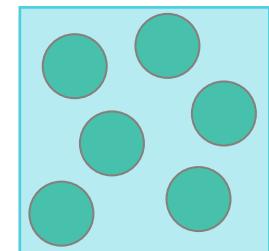
in-situ forming depot



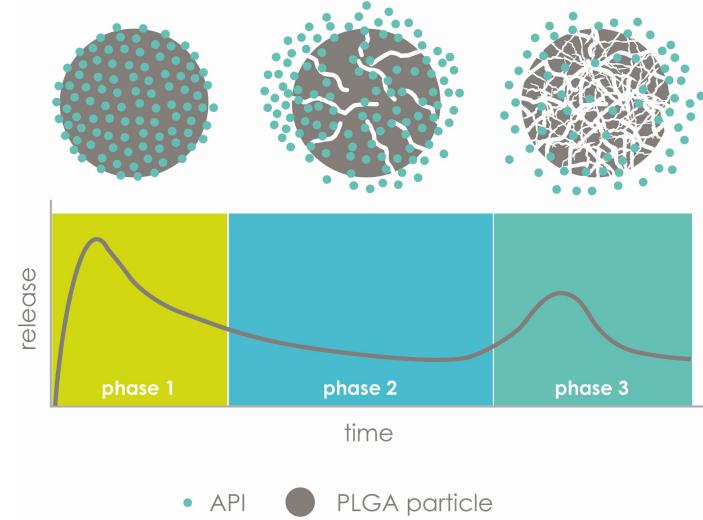
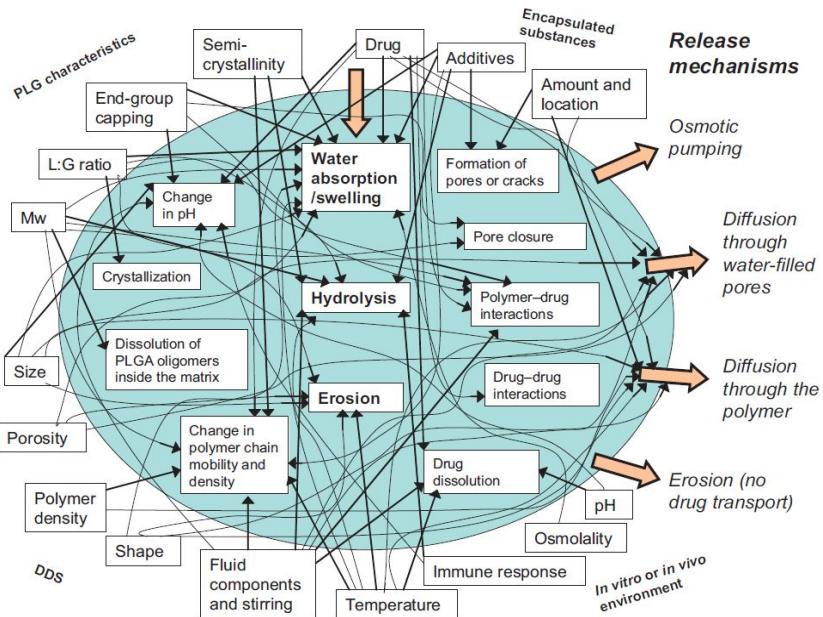
nanoparticles



microparticles



# PLGA formulation degradation mechanisms



# polymer thermal properties can alter choice of formulation process

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polymer	Tg (°C)	Tm (°C)	structure	
PGA	35 – 45	220-233	Semi-crystalline	
PLGA	35 – 55	Amorphous	Amorphous	
PDLLA	45 – 60	Amorphous	Amorphous	
PLCL	10 - 20	130 - 155	Amorphous	
PCL	-65 to -60	55 - 65	Semi-crystalline	

increasing  
degradation  
timeframe



# API can alter choice of formulation process

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## API type

- organic small molecule
- protein
- peptide
- monoclonal antibody
- DNA / RNA

## solubility

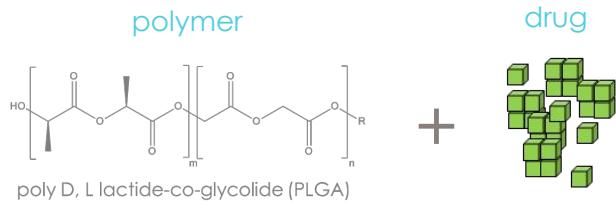
- hydrophobic vs. hydrophilic vs. amphiphilic
- water solubility

## dosage requirements and duration

- therapeutic level
- possibility for increased bioavailability vs. current dosing



# hot melt extrusion process



1

common feed issues: feeding rate, static, flow, clogging, drug / PLGA dispersion

## how can we improve HME performance of PLGA?

- dense flowing particles
- flexible particle size for drug / PLGA dispersion
- tune process parameters and optimise

extrusion temperature

3

poor content uniformity  
in extrudate

2

degradation due to excessive thermal and shear stress

# PLGA form enhancement for HME

Avg. particle diameter (µm)	Max. particle diameter (µm)	Min. particle diameter (µm)
351	1326	10.3



PLGA fine particles

Avg. particle diameter (µm)	Max. particle diameter (µm)	Min. particle diameter (µm)
2795	4230	2106



PLGA coarse granules



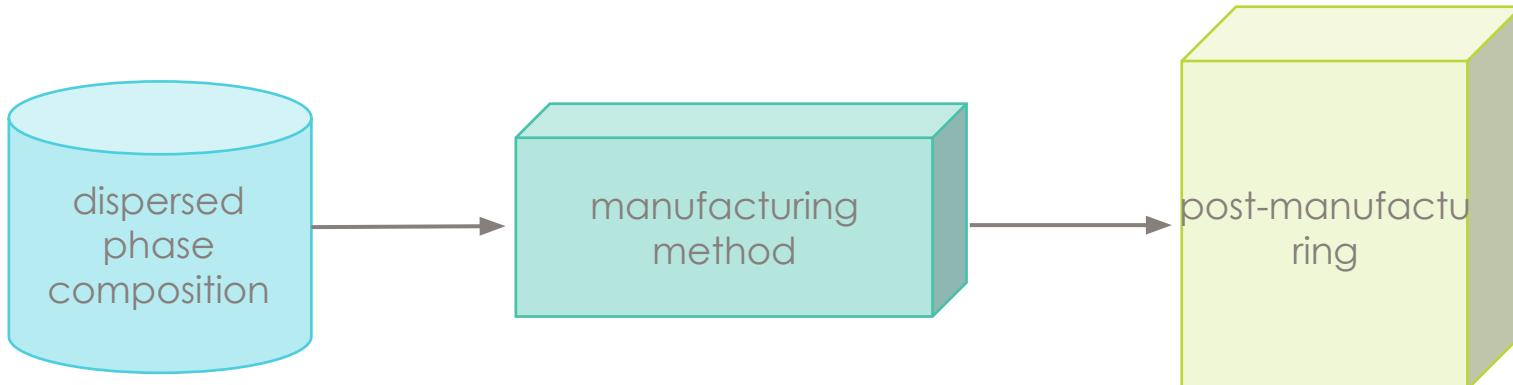
\*\*\* Data obtained via Light Microscopy inspection. Sample size of 100 particles used for each case \*\*\*

## fine particles improve HME formulations

- through multiple studies, it was determined that fine particles provide better mixing and decreased molecular weight reduction during melting process

# microsphere process

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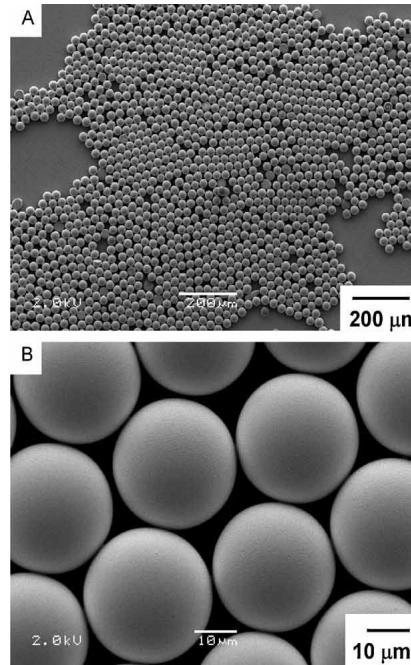


# particle technologies

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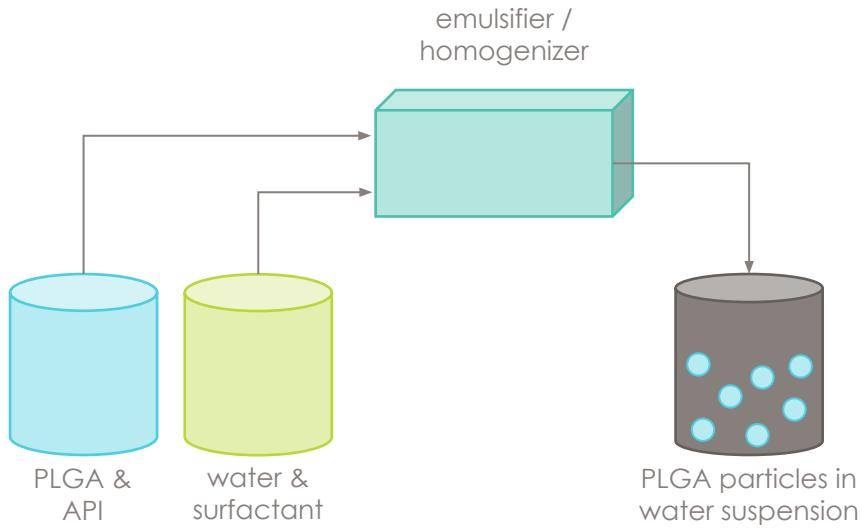
- single / double emulsions
- coacervation
- spray drying
- microfluidics
- membrane emulsification
- nano-precipitation
- vibration assisted printing
- self-assembly (micelle tech)
- electro-spinning / electro-spraying

+ downstream handling



# single emulsion

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## pros

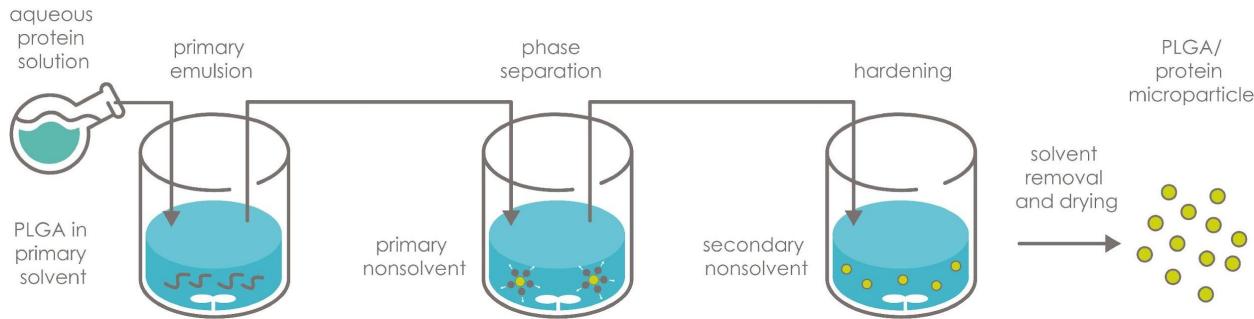
- production of large quantities very quickly and easily
- control of precipitation rate, which effects the release profile

## cons

- advantageous to use organic solvents with least water solubility
- requires ability to process quickly downstream due to large volumes
- large quantities of waste

# coacervation

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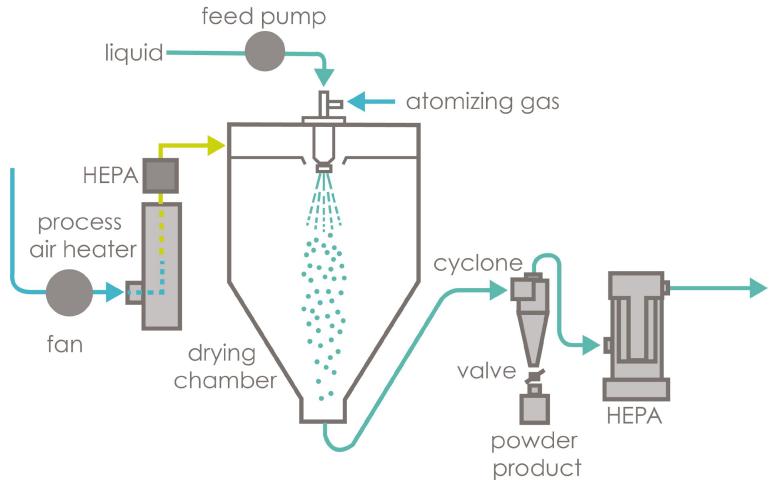
## pros

- high encapsulation of hydrophilic drugs
- limited total waste quantity

## cons

- use of and disposal of explosive hazardous organic solvents
- challenges in scale-up
  - time factor of transferring into non-solvents
  - stirring dynamics different with larger equipment

# spray drying



## pros

- high encapsulation of hydrophilic drugs, with caveat that water is not advantageous to use
- more uniform particle size distribution
- can utilize any volatile organic solvent, including acetone
- produces a solid powder with low residual organic solvents and no down-stream processing is needed

## cons

- slow process
- manufacturing:
  - custom spray dryers must be made to fit each project's aseptic process/requirements
  - cleaning equipment for re-use

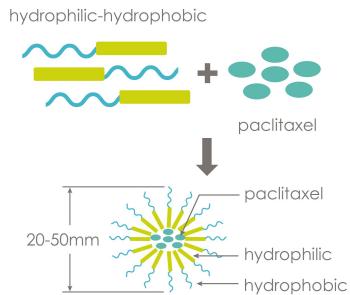
# nanoparticle & hydrogels

## rational

- increased stability, reduced toxicity
- + penetration ability, smart targeting using polymer

## examples

- Genexol\*
- mAb loaded nanoparticles



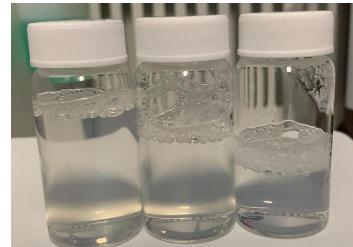
	Genexol®PM	Conventional paclitaxel
API	Paclitaxel 30mg	Paclitaxel 30mg
Solubilizer	mPEG-PDLLA* 150 mg	Cremophor 2,645mg
MTD	390 mg/m <sup>2</sup>	175 mg/m <sup>2</sup>
Character	<ul style="list-style-type: none"><li>• Improved solubility</li><li>• Reduced toxicity</li><li>• Improved efficacy</li><li>• Reduced hypersensitivity</li></ul>	<ul style="list-style-type: none"><li>• Low MTD</li><li>• Cremophor induced<ul style="list-style-type: none"><li>- Toxicity</li><li>- Hypersensitivity reaction and neuropathy</li></ul></li></ul>

## tri-block polymer rational

- water rich matrix to support structure of large molecules & cells
- does not require harsh processing (no org. solvents or temperature)

## example

- thermosensitive hydrogels based on tri-block copolymer structure



0 – 25 °C = solution



30 – 40 °C = hydrogel



# common challenges

## chemistry

- o how do I select appropriate polymer for project target and how to optimise?
- o drug depot performance versus process needs

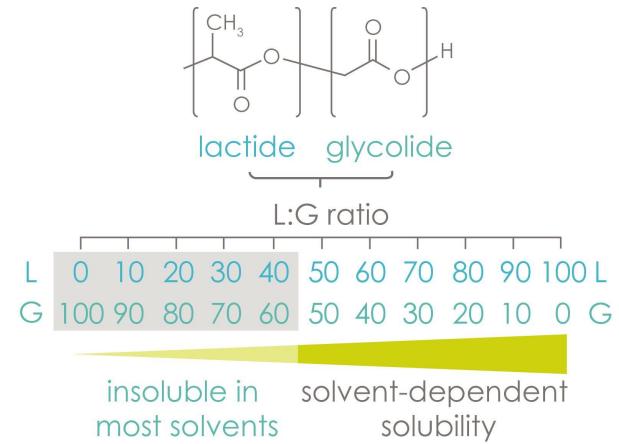
## formulation

- o weighing pros – cons of formulation formats that exist
- o solvent based technologies
  - solvent compatibility is chemistry and drug dependant
  - solvent impact on formulation

## terminal sterilization

- o options, pros vs. cons and typical approaches
- o accounting for sterilization impacts

many project specific challenges!



# summary

## relevant excipients

- viatel™ bioresorbable polymers
- aqualon™ CMC BET
- pharmaSOLVE™ NMP (N-methyl-2-pyrrolidone)

## technical support

- 70+ off-the-shelf viatel™ bioresorbable polymers grades
- custom polymer synthesis
  - monomer choice
  - end-cap
  - molecular weight (inherent viscosity)
  - branched / armed polymers



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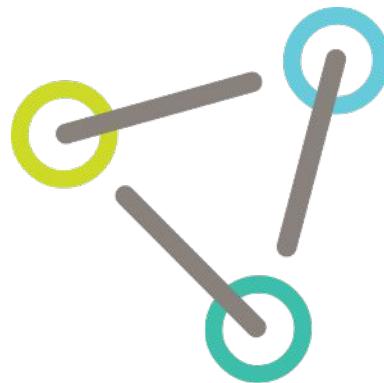
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